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Submission to Microchemical Journal - manuscript number

1 message

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Reply-To: Microchemical Journal <microc@elsevier.com>
To: Andi Dian Permana <andi.dian.permana@farmasi.unhas.ac.id>

Tue, Jul 6, 2021 at 12:07 AM

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Manuscript Number: MICROC-D-21-01793

New and Rapid HPLC-UV analytical method for quantification of metronidazole: Application to ex vivo ocular kinetic assessments following the application of thermosensitive ocular in situ gel

Dear Dr. Permana,

Your above referenced submission has been assigned a manuscript number: MICROC-D-21-01793.

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REVIEWERS**

Decision on submission to Microchemical Journal

1 message

Microchemical Journal <em@editorialmanager.com>
Reply-To: Microchemical Journal <support@elsevier.com>
To: Andi Dian Permana <andi.dian.permana@farmasi.unhas.ac.id>

Wed, Sep 22, 2021 at 2:47 PM

Manuscript Number: MICROC-D-21-01793

New and Rapid HPLC-UV analytical method for quantification of metronidazole: Application to ex vivo ocular kinetic assessments following the application of thermosensitive ocular in situ gel

Dear Dr. Permana,

Thank you for submitting your manuscript to Microchemical Journal.

I have completed my evaluation of your manuscript. The reviewers recommend reconsideration of your manuscript following major revision. I invite you to resubmit your manuscript after addressing the comments below. Please resubmit your revised manuscript by Nov 21, 2021.

When revising your manuscript, please consider all issues mentioned in the reviewers' comments carefully: please outline every change made in response to their comments and provide suitable rebuttals for any comments not addressed. Please note that your revised submission may need to be re-reviewed.

To submit your revised manuscript, please log in as an author at <https://www.editorialmanager.com/microc/>, and navigate to the "Submissions Needing Revision" folder.

Microchemical Journal values your contribution and I look forward to receiving your revised manuscript.

Kind regards,

Justyna Płotka-Wasyłka
Editor
Microchemical Journal

Editor and Reviewer comments:

Reviewer 1: The authors presented HPLC-UV method for quantification of metronidazole and its application. The language of article is very poor. Introduction section is too large. There are so many spelling mistakes in the entire paper. Kindly do necessary changes. Please resubmit the entire paper after appropriate corrections.

1. Application word repeated in the title of the manuscript. Kindly reframe it.
2. Kindly remove rapid word from the title because there are so many papers on metronidazole which has lower chromatographic run time compared to the present method.
3. Spelling mistake in line no. 43, Kindly correct it. i.e. "nd". It is actually "and".
4. Kindly use multiplication symbol instead of X in the column dimension.
5. Literature is incomplete. Kindly cite some paper which has used HPLC and LC-MS/MS for the quantification of metronidazole in various biological matrices.

Reviewer 2: 1. In the abstract: However, its effectiveness has been hampered by several limitations of eye drop preparations due to rapid elimination from the eye", this sentence signifies that several limitations are only due to "rapid elimination", which is not true, correction in this sentence is needed. Line 51: what is ocular "cokinetics"? Put the Trade Mark on "Xselect" CSHTM C18 HPLC column, like Xselect™.

2. In highlights, what does it mean "ex vivo HPLC method", I do not think we should call it ex vivo, it is simple HPLC analytical method.
3. The Poloxamers used to prepare the thermo sensitive in situ ocular gels is not new (although the method

development for metronidazole for ocular use can give a little novelty). Therefore, the formulations and findings in the present study are different from the previous reports where these polymers were used for ocular application. Justify your findings in comparison to the previous reports with proper references such as:

PMID: 20500130 or DOI: 10.3109/10717544.2010.483255

PMID: 9519158 or DOI: 10.1021/js970090e

<https://www.sciencedirect.com/science/article/pii/S1319016420301523>

4. Page 9, line 240: As mentioned "The treated cornea was then placed between the chambers in the diffusion cells", what was the treatment of the cornea? I think here freshly excised cornea not the treated one was used. Line 244: What do you mean by "Kornea"?
5. In the equations of LOD and LLOQ, specify the term "Syx". Mention the values in the text also.
6. Line 171-172: what was the v/v ratio of the mobile phase mixture (acetonitrile and 20 mM acetate buffer)?
7. Line 297: I think, the unit of time in the value 61.33 is missing.
8. In Table S3. Mention the unit of excipients used.
9. Line 226-227: "2.6 Application of validated HPLC method to assess ocular kinetics evaluation of formulated from thermosensitive gel formulation" recheck this subheading.
10. Mention all the excipients with exact weights used in the preparation of stimulated tear fluid.
11. Although the main of this work is the development and validation of a new and rapid HPLC-UV analytical method for metronidazole quantification, then maximum data and tables related to method validation should be presented in the main manuscript rather than in Supplementary files.
12. The drug was analyzed only in the corneal extract, so it is better to mention in the manuscript that the thermosensitive ocular gel improved metronidazole concentration in corneal tissues rather than "ocular tissue", because ocular tissue includes iris, conjunctiva, retina etc.

Data in Brief (optional):

We invite you to convert your supplementary data (or a part of it) into an additional journal publication in Data in Brief, a multi-disciplinary open access journal. Data in Brief articles are a fantastic way to describe supplementary data and associated metadata, or full raw datasets deposited in an external repository, which are otherwise unnoticed. A Data in Brief article (which will be reviewed, formatted, indexed, and given a DOI) will make your data easier to find, reproduce, and cite.

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 **10 Micro_Comments to the Authors & Editor.docx**
15K

**BUKTI
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Confirming submission to Microchemical Journal

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Microchemical Journal <em@editorialmanager.com>
Reply-To: Microchemical Journal <support@elsevier.com>
To: Andi Dian Permana <andi.dian.permana@farmasi.unhas.ac.id>

Mon, Sep 27, 2021 at 12:45 AM

This is an automated message.

Manuscript Number: MICROC-D-21-01793R1

New HPLC-UV analytical method for quantification of metronidazole: Application to ex vivo ocular kinetic assessments following the administration of thermosensitive ocular in situ gel

Dear Dr. Permana,

We have received the above referenced manuscript you submitted to Microchemical Journal.

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Microchemical Journal

New HPLC-UV analytical method for quantification of metronidazole: Application to ex vivo ocular kinetic assessments following the administration of thermosensitive ocular in situ gel

--Manuscript Draft--

Manuscript Number:	MICROC-D-21-01793R1
Article Type:	Research Paper
Section/Category:	Chromatography and separation techniques
Keywords:	Metronidazole; keratitis; HPLC; thermosensitive in situ gel; ocular kinetic; Method Validation
Corresponding Author:	Andi Dian Permana INDONESIA
First Author:	Nur Asma
Order of Authors:	Nur Asma Nurul Muhlisah Maddeppungeng Muhammad Raihan Arini Putri Erdiana Achmad Himawan Andi Dian Permana
Abstract:	<p>Metronidazole eye drops have been used to treat Acanthamoebakeratitis. However, ophthalmic preparations also have some limitations, one of which is the rapid elimination of the drug, that reducing the effectiveness of the drug. Accordingly, an alternative delivery approach can be applied to overcome this issue. Additionally, as one of critical steps in the formulation development, analytical methods that allow the quantification of metronidazole in ex vivo corneal permeation and deposition should also be developed. Here, we report a validated high-performance liquid chromatography method (HPLC-UV) according to ICH guidelines for the measurements of metronidazole concentrations following formulation of thermosensitive ocular in situ gel and its administration in ex vivoporcine corneas. The development of extraction techniques and optimization of HPLC conditions were optimized using analytical quality by design. Xselect™ CSHTM C18 HPLC column (Water, 3.0 × 150 mm, particle size 3.5 m) was used to separate all analytes by isocratic elution with mobile phases of acetate buffer and acetonitrile with LLOQ value of 0.08 µg/mL. The resulting method proved to be selective, precise, and accurate and was successfully applied to determine ocular kinetic profiles of metronidazole from thermosensitive ocular in situ gel in ex vivoporcine corneas, showing that this approach was able to improve the concentration of metronidazole in the corneal tissues. We, therefore, suggested that HPLC-UV approach developed in this study has the potential to be used in drug release evaluation, therapeutic drug control research, ocular kinetics, and toxicological evaluation.</p>



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HASANUDDIN UNIVERSITY
FACULTY OF PHARMACY

Alamat Jalan Perintis kemerdekaan Km.10, Makassar 90245
Telepon (0411) 588556, Faksimili (0411) 590663
Laman: farmasi@unhas.ac.id

The Editor
Microchemical Journal

September 26, 2021

Dear Sir/Madam,

I wish you to consider our manuscript for publication in *The Microchemical Journal*. Following the reviewer comments, we have changed our title from “**New and rapid HPLC-UV analytical method for quantification of metronidazole: application to *ex vivo* ocular kinetic assessments following the application of thermosensitive ocular in situ gel**” to “**New HPLC-UV analytical method for quantification of metronidazole: Application to *ex vivo* ocular kinetic assessments following the administration of thermosensitive ocular *in situ* gel**”.

Importantly, we have addressed all comments from all reviewers as shown in “Response to Reviewer” file. Also, we have corrected all technical issues in our manuscript.

The manuscript has not been previously published in any language anywhere and it is not under simultaneous consideration by another journal. We have no conflicts of interest.

We appreciate your attention. We hope you will now consider publishing our research in *The Microchemical Journal* and look forward to hearing from you in due course.

Yours Sincerely,

Andi Dian Permana (on behalf of all authors)
Faculty of Pharmacy, Hasanuddin University, Indonesia
Email: andi.dian.permana@farmasi.unhas.ac.id

Manuscript Number: MICROC-D-21-01793

New and Rapid HPLC-UV analytical method for quantification of metronidazole: Application to ex vivo ocular kinetic assessments following the application of thermosensitive ocular in situ gel

Response to Reviewers

We are very thankful to the reviewers for taking the time to provide helpful comments for improvements for our manuscript. We have addressed each of the reviewers' comments in detail below.

Reviewer 1

The authors presented HPLC-UV method for quantification of metronidazole and its application. The language of article is very poor. Introduction section is too large. There are so many spelling mistakes in the entire paper. Kindly do necessary changes. Please resubmit the entire paper after appropriate corrections.

Response to Reviewer

We thank the Reviewer for noticing our spelling mistakes and the large Introduction. We deliberately corrected our poor language and deleted some sentences that we considered not necessary for the article. We believe that the English of our manuscript has now been improved significantly.

Comments to the Author:

1. Application word repeated in the title of the manuscript. Kindly reframe it.
2. Kindly remove rapid word from the title because there are so many papers on metronidazole which has lower chromatographic run time compared to the present method.

Response to Reviewer

We thank the reviewer for this valuable suggestion. We have reframe the title so that the repeating word is avoided. We have also removed the word 'rapid' as we also agree that our method is comparable to previous studies.

3. Spelling mistake in line no. 43, Kindly correct it. i.e. "nd". It is actually "and".

Response to Reviewer

Thank you for your suggestion. We have corrected the misspelling word.

4. Kindly use multiplication symbol instead of X in the column dimension.

Response to Reviewer

We thank the Reviewer for suggesting all the detail in our manuscript. We noticed the mistake and change X in the column dimension to \times

5. Literature is incomplete. Kindly cite some paper which has used HPLC and LC-MS/MS for the quantification of metronidazole in various biological matrices.

Response to Reviewer

Thank you for your suggestion. We have added some literatures in Introduction.

Reviewer 2

Comment to authors:

1. In the abstract:

a. However, its effectiveness has been hampered by several limitations of eye drop preparations due to rapid elimination from the eye", this sentence signifies that several limitations are only due to "rapid elimination", which is not true, correction in this sentence is needed.

Response to Reviewer

We thank reviewers for this valuable suggestion. We have revised the sentences to address your concerns and hope that it is now clearer. We have changed "However, its effectiveness has been hampered by several limitations of eye drop preparations due to rapid elimination from the eye" to "However, ophthalmic preparations also have some limitations, one of which is the rapid elimination of the drug, that reducing the effectiveness of the drug."

b. Line 51: what is ocular "cokinetics"? Put the Trade Mark on "Xselect" CSHTM C18 HPLC column, like Xselect™.

Response to Reviewer

Thank you for your suggestion. We have corrected the misspelling word that contain "cokinetics" to "kinetics" and put the Trade Mark on Xselect.

2. In highlights, what does it mean "ex vivo HPLC method", I do not think we should call it ex vivo, it is simple HPLC analytical method.

Response to Reviewer

We thank reviewers for this valuable suggestion. We have revised the sentences to address your concerns and hope that it is now clearer.

3. The Poloxamers used to prepare the thermo sensitive in situ ocular gels is not new (although the method development for metronidazole for ocular use can give a little novelty). Therefore, the formulations and findings in the present study are different from the previous reports where these polymers were used for ocular application. Justify your findings in comparison to the previous reports with proper references such as:

PMID: 20500130 or DOI: 10.3109/10717544.2010.483255

PMID: 9519158 or DOI: 10.1021/js970090e

<https://www.sciencedirect.com/science/article/pii/S1319016420301523>

Response to Reviewer

We thank reviewers for this valuable input. Indeed, Poloxamers is not new in the field of thermosensitive preparation and thus, we agree to incorporate the suggested articles on our manuscript draft. We have read the articles and justified our findings using the suggested citations. More specifically, we have added the our justification in the line 416-420 and 446-457. We again highly appreciated the suggestion of the reviewers in improving the quality of this work.

4. Page 9, line 240: As mentioned "The treated cornea was then placed between the chambers in the diffusion cells", what was the treatment of the cornea? I think here freshly excised cornea not the treated one was used. Line 244: What do you mean by "Kornea"?

Response to Reviewer

We thank the Reviewer for this question. In this study, the treated cornea determined by freshed cornea with a scleral tissue size of 2-4 mm then washed with cold normal saline. To avoid misconception we change the "treated" word. There was spelling mistake in the line 244. We have clarified this in the method.

5. In the equations of LOD and LLOQ, specify the term "Syx". Mention the values in the text also.

Response to Reviewer

We thank the Reviewer for pointing this out. In the measurement of LOD and LOQ, the value were expressed as $3.3 \times Syx/b$ and $10.0 \times Syx/b$, respectively, where Syx is residual variance due to regression and b is the mean slope of the linear regression curves. We have clarified this in the method.

6. Line 171-172: what was the v/v ratio of the mobile phase mixture (acetonitrile and 20 mM acetate buffer)?

Response to Reviewer

We thank the Reviewer for reviewing the manuscript in detail and giving the comments about the v/v ratio of mobile phase. There are 3 variable that we use to optimize the chromatographic conditions including mobile phase, flow rate, mobile phase pH, and acetonitrile concentration. The optimized using The Composite Central Design (CCD) under response surface methodology, as we can see in the supplementary section Table S2 for Acetonitrile concentration.

7. Line 297: I think, the unit of time in the value 61.33 is missing.

Response to Reviewer

We thank you Reviewer for reviewing our manuscript in detail. We rewrote the sentence to improve its clarity.

8. In Table S3. Mention the unit of excipients used.

Response to Reviewer

We thank the reviewer for pointing this out. We added the unit of excipient used as (% w/v).

9. Line 226-227: "2.6 Application of validated HPLC method to assess ocular kinetics evaluation of formulated from thermosenstivie gel formulation" recheck this subheading.

Response to Reviewer

We thank the Reviewer for informing us to recheck the subheading. We realized that the previous subheading was not quite right so we changed the subheading to "Optimization and ocular kinetics evaluation of formulated metronidazole gels"

10. Mention all the excipients with exact weights used in the preparation of stimulated tear fluid.

Response to Reviewer

We thank the Reviewer for reviewing the manuscript in detail and giving the comments about all the excipients with exact weights used in the preparation of stimulated tear fluid. In this study, simulated tear fluid consisting of 6.7 g NaCl, 2.0 g NaHCO₃ and 0.08 g CaCl₂·2H₂O was intially prepared by dissolving all components in 1 L deionized water (final pH of 7.4). We have clarified this in the method.

11. Although the main of this work is the development and validation of a new and rapid HPLC-UV analytical method for metronidazole quantification, then maximum data

and tables related to method validation should be presented in the main manuscript rather than in Supplementary files.

Response to Reviewer

We thank the Reviewer for reviewing the manuscript in detail and giving the comments about our validation tables. We combined Table S8, S9, S10 that related to method validation with Table 1 in the main manuscript, respectively.

12. The drug was analyzed only in the corneal extract, so it is better to mention in the manuscript that the thermosensitive ocular gel improved metronidazole concentration in corneal tissues rather than "ocular tissue", because ocular tissue includes iris, conjunctiva, retina etc.

Response to Reviewer

We would like to thank the Reviewer for the comments. Following the comments, we have changed "ocular tissue" to "corneal tissue" in our manuscript.

Highlights:

- We developed HPLC method of metronidazole for quantification in corneal tissue
- We validated the HPLC method according ICH guidelines
- We successfully applied the method in *ex vivo* ocular kinetic assay
- Thermosensitive ocular gel improved metronidazole concentration in ocular tissue

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1 **New HPLC-UV analytical method for quantification of metronidazole: Application to *ex vivo***
2 **ocular kinetic assessments following the administration of thermosensitive ocular *in situ* gel**

3
4 Nur Asma¹, Nurul Muhlisah Maddeppungeng¹, Muhammad Raihan², Arini Putri Erdiana³,
5 Achmad Himawan³, Andi Dian Permana^{3*}

- 6
7 1. Department of Pharmacy, Faculty of Medicine and Health Sciences Faculty, Alauddin
8 Islamic State University, Samata Gowa, 92113, Indonesia
9 2. Department of Phytochemistry, Faculty of Pharmacy, Hasanuddin University, Makassar,
10 90245, Indonesia
11 3. Department of Pharmaceutics, Faculty of Pharmacy, Hasanuddin University, Makassar,
12 90245, Indonesia

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14 ***Corresponding author:**
15 Andi Dian Permana
16 Faculty of Pharmacy, Hasanuddin University, Indonesia
17 Email: andi.dian.permana@farmasi.unhas.ac.id

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34 **Abstract**

35 Metronidazole eye drops have been used to treat *Acanthamoeba* keratitis. However, ophthalmic
36 preparations also have some limitations, one of which is the rapid elimination of the drug, that
37 reducing the effectiveness of the drug. Accordingly, an alternative delivery approach can be
38 applied to overcome this issue. Additionally, as one of critical steps in the formulation
39 development, analytical methods that allow the quantification of metronidazole in *ex vivo* corneal
40 permeation and deposition should also be developed. Here, we report a validated high-performance
41 liquid chromatography method (HPLC-UV) according to ICH guidelines for the measurements of
42 metronidazole concentrations following formulation of thermosensitive ocular *in situ* gel and its
43 administration in *ex vivo* porcine corneas. The development of extraction techniques and
44 optimization of HPLC conditions were optimized using analytical quality by design. Xselect™
45 CSHTM C18 HPLC column (Water, 3.0 × 150 mm, particle size 3.5 m) was used to separate all
46 analytes by isocratic elution with mobile phases of acetate buffer and acetonitrile with LLOQ value
47 of 0.08 µg/mL. The resulting method proved to be selective, precise, and accurate and was
48 successfully applied to determine ocular kinetic profiles of metronidazole from thermosensitive
49 ocular *in situ* gel in *ex vivo* porcine corneas, showing that this approach was able to improve the
50 concentration of metronidazole in the corneal tissues. We, therefore, suggested that HPLC-UV
51 approach developed in this study has the potential to be used in drug release evaluation, therapeutic
52 drug control research, ocular kinetics, and toxicological evaluation.

53 **Keywords:**

54 Metronidazole, keratitis, HPLC, thermosensitive *in situ* gel, ocular kinetic, method validation

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1. Introduction

Infection that presents with corneal ulcerations known as *Acanthamoeba* keratitis is caused by *Acanthamoeba* species. It was first reported in 1973. This condition occurs commonly when someone uses a contact lens washing solution prepared with non-sterile salt tablets and water [1].

Metronidazole is a derivative of 5-Nitroimidazole known to act as a powerful antibacterial and antiprotozoal. For decades, eye preparations has become a fast growing pharmaceutical technology [2]. In ophthalmology, general eye drops and topical eye preparations are the most widely used preparations. It is considered the most efficient form of treating infections of the foreground structures generally caused by anaerobic bacteria [3]. *Acanthamoeba* keratitis can be treated using 0.5% metronidazole eye drops mixed with other antiprotozoal preparations [4]. Metronidazole eye drops have long been a formulary drug in pharmacies as an alternative to the lack of a commercially available form of eye medications. In ophthalmology, preparations with 0.1% and 0.5% metronidazole solutions have been used to treat *Acanthamoeba* keratitis [5–7].

Topical administration of the drug is more prevalent among patients and safer than the intraocular injection, but topical use of this drug has the disadvantage that the drug cannot be adequately absorbed in the eye and reaches the posterior segment. As a part of trends in topical formulation, thermosensitive gels have been utilized in overcoming these problems. The term thermosensitive refers to its ability to form gel or solution reversibly upon at a particular temperature. This can be achieved by taking advantages of unique properties of some gelling agent such as N-acrylamide based co-polymers and poly(propylene oxide) (PPO)/ polyethylene oxide (PEO) block co-polymers [8]. However, previous reports showed that combination of two co-polymers or its interaction with other gelling agents is required to obtained a relatively precise temperature for the gel to form [9–11]. To our best understanding, this is the first time the technology of thermosensitive gels is applied to administer metronidazole in an ocular drug delivery. Therefore, it is also an important task to assess whether the newly incorporated gel bases is able to release metronidazole upon application in the eye condition.

Over the last few decades, many improved methods have been undertaken to find and explore more effective ways of administering eye medications and treatments for various eye diseases [12]. In transcorneal penetration studies, *in vitro* cell culture models have been widely selected. The development of an organotypic corneal construction technique also studies the

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4 96 bioavailability of ophthalmic drugs using primary cell cultures and immortalized cell lines. There
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6 97 is great potential for research into corneal penetration in artificially cultivated human corneas.
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8 98 Using a research model using cut animal corneal tissue to study drug penetration is one technique
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10 99 with promising results, although it is necessary to consider the significant variation between
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12 100 species [13]. One of the developments in the new *ex vivo* model is to use a porcine cornea disc. It
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14 101 is considered to be more cost-effective for candidates for transcorneal penetrating topical therapy
15 102 [14].

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17 103 Method development and validation have tremendous importance in the QC of the drug. In
18
19 104 recent years because of its importance, the development of new testing methods for drug
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21 105 determination has received considerable attention in determining potency of active ingredients in
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23 106 eye drops. Hence, HPLC is the analytical method of choice for measuring metronidazole [7]. The
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25 107 HPLC method validation test will be conducted according to guidelines recommended by the
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27 108 USFDA (2001) [15]. Comparison between the retention times of metronidazole detected in the
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29 109 drug-free plasma assay and metronidazole derived from drug injection extracted from spiked
30 110 plasma will be investigated as a test of specificity and selectivity [7].

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32 111 Several previous studies related to HPLC and LC-MS/MS for the quantification of
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34 112 metronidazole in various biological matrices have been carried out. A study by Silva et al (2009)
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36 113 showed simple, fast, sensitive, and selective results using liquid chromatography (LC)-tandem
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38 114 mass spectrometry (MS-NONA)[16]. In addition, HPLC and LC-MS/MS for metronidazole
39 115 quantification have also been performed on saliva, plasma, and gingival crevicular fluid [17].

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41 116 Transcorneal penetration of metronidazole using *ex vivo* porcine corneal model has never
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43 117 been developed. The development of extraction method before having HPLC assay is essential to
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45 118 produce maximum drug concentration. Optimization and development of analytical methods, also
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47 119 recognized as the analytical quality by design (AQbD), are now widely applied to quality by design
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49 120 (QbD). This concept is considered necessary since the first time it was first introduced by the
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51 121 USFDA [18]. This concept is known to require less time for experimentation because it uses the
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53 122 experimental design method (DOE) to obtain possible combinations of parameters and has also
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55 123 been recommended in robustness testing [18,19]. Implementation of AQbD applications in HPLC
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57 124 method development has been done in many studies, Rozet et al reported using AQbD approach
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59 125 for analytical method by HPLC [20]. Prior to analyzing metronidazole with HPLC, we developed
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61 126 an optimised method for extracting drug form matrix using various sonication time and stirring

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4 127 time. This aimed to maximise the number of metronidazole that were measured using HPLC
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6 128 method. The validated HPLC method will be used to assess the *ex vivo* ocular kinetics of the drug
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8 129 after topical application to the eye.
9

10 130 11 131 **2. Materials and methods**

12 131 13 132 **2.1. Chemicals and materials**

14 132
15 133 Metronidazole ($\geq 99.9\%$, purity), analytical grade trifluoroacetic acid, and HPLC-grade
16
17 134 Methanol (MeOH) (Sigma-Aldrich Pte Ltd, Singapore), Xselect CSH™ C₁₈ HPLC column
18
19 135 (particle size 3.5 μm , 3, 0 \times 150 mm; Waters, Dublin, Ireland), chemical reagent (Sigma - Aldrich
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21 136 Pte Ltd, Singapore). Other reagents were analytical grade and obtained from standard commercial
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23 137 supplier.
24

25 138 26 139 **2.2. Stock Preparation, Calibration Standards and Quality Control Samples**

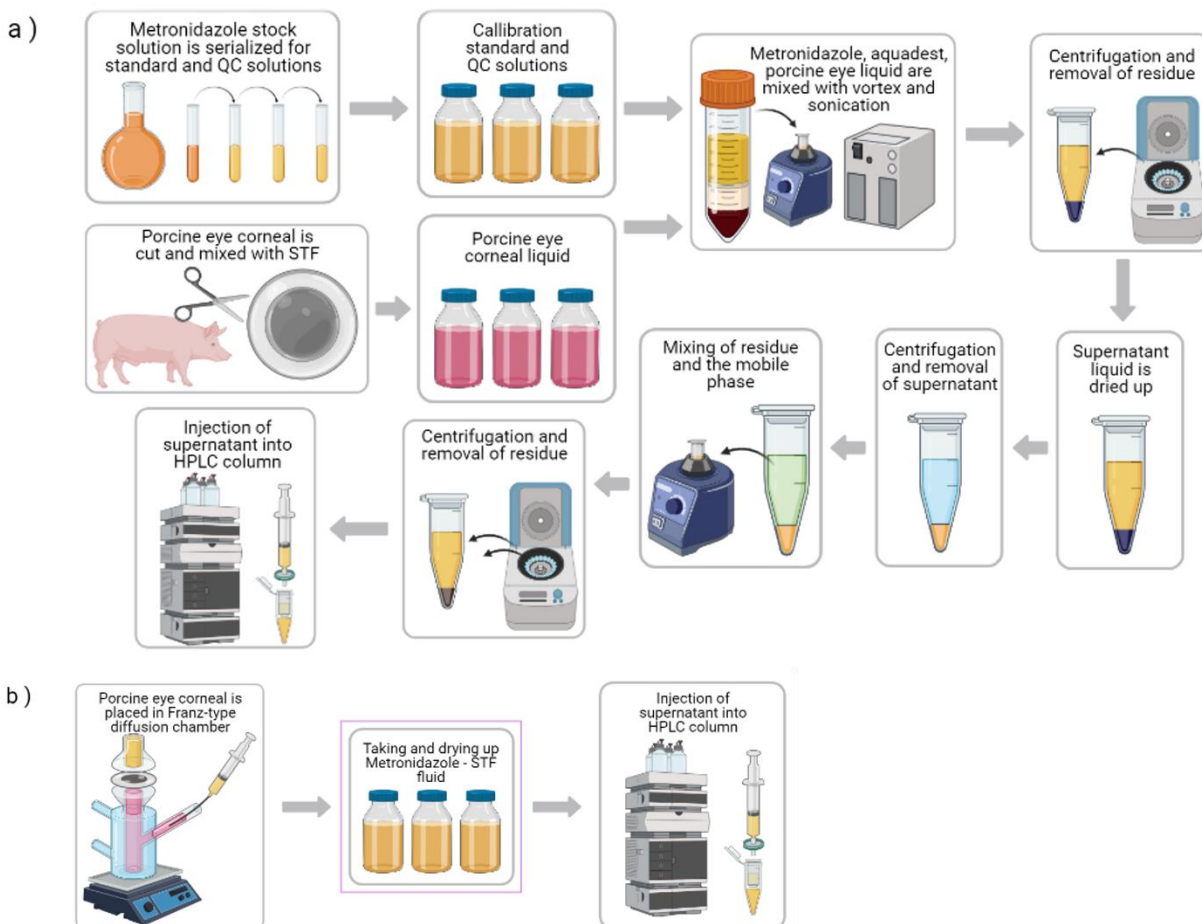
27 139
28 140 Metronidazole stock solution was prepared by dissolving 50 mg in 50 ml methanol so that
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30 141 a concentration of 1 mg/mL was obtained. The working solutions were diluted into serial
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32 142 concentrations for standard calibration, and quality control (QC) solutions. In the calibration of the
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34 143 test method, a concentration series was made using the stock solution diluted with porcine eye
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36 144 corneal tissue matrices. The final concentrations obtained ranged from 0.01 to 10 $\mu\text{g/mL}$. QC
37
38 145 solutions were made in three types of concentrations, namely 0.15 $\mu\text{g/mL}$, 3.5 $\mu\text{g/mL}$ and 7.5
39
40 146 $\mu\text{g/mL}$ for low QC, medium QC and high QC, respectively. All QC solutions were prepared in
41
42 147 porcine eye corneal tissue matrices.
43

44 148 45 149 **2.3. Preparation and Analytes Extraction of Samples**

46 150 Simulated tear fluid consisting of 6.7 g NaCl, 2.0 g NaHCO₃ and 0.08
47
48 151 g CaCl₂·2H₂O was initially prepared by dissolving all components in 1
49
50 152 L deionized water (final pH of 7.4). Preparation of the sample was conducted by mixing porcine
51
52 153 eye corneal 2,5 g with 2,5 g STF (stimulated tear fluid) pH 7,4 to make porcine eye corneal fluid,
53
54 154 2 mg of metronidazole was added with 2 mL aquadest. The 100 μL of the mixture was centrifuged
55
56 155 with 900 μL porcine eye corneal fluid. The extraction volume, stirring time and sonication time
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58 156 were evaluated. The response surface methodology to optimize sonication time, vortex time, and
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60 157 methanol volume (**Table S1**) used Composite Central Design (CCD) by Design Expert Software
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4 158 version 11 (State-Ease, Minneapolis, MN, USA). The response parameters were extraction
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6 159 performance and fluid evaporation time.

7
8 160 The supernatant liquid was put into a small glass container and then dried up in a fume
9
10 161 hood for about 3 hours. This is done in order to obtain dried residue. The residual mixture and the
11
12 162 100 μL mobile phase were stored in a 0.5 mL centrifuge tube. For 30 seconds, the mixture was
13
14 163 stirred and then rotated at 14,000 rpm \times g for 15 minutes. A total of 10 μL of the treated supernatant
15
16 164 solution was injected into the HPLC column. The work steps are illustrated in **Figure 1**.



49 166
50 167 **Figure 1.** Illustration of the work steps
51 168

52 169 **2.4. Instrumentation and Optimisation of HPLC–UV conditions**

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54 170 Simultaneous analysis of the entire analyte applied using HPLC system (Shimadzu
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56 171 Prominence, Shimadzu, Kyoto, Japan) equipped with PDA detector; acetonitrile and 20 mM
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acetate buffer were utilized as the mobile phases; the separation of analytes using Xselect CSH™ C18 column (Waters, 3.0 × 150 mm); 3.5 μm particle size with guard cartridge. CCD was used in the response surface methodology to optimize mobile phase, flow rate, mobile phase pH, and acetonitrile concentration (**Table S2**). Design Expert® Software version 11 (State-Ease, Minneapolis, MN, USA) was used in processing the data and performed statistical analyses. Parameters recorded response were the retention time (RT), the theoretical plates and tailing factors.

2.5. Analytical method validation

Based on US FDA and ICH guidelines, the developed bioanalytical method was validated [15,18]. Validated parameters were precision, accuracy, linearity, selectivity, carry over, extraction recovery, lower limit of quantification (LLOQ), dilution integrity, and stability.

2.5.1. Linearity, LOD and LLOQ

Linearity was measured by a calibration curve derived from a sample with a working standard solution. The calibration curve was made of seven levels of concentration with three separate times.

The limits of detection and limits of quantification were determined by the regression of the obtained standard curves. LOD and LOQ were represented as $3.3 \times S_{yx}/b$ and $10.0 \times S_{yx}/b$, respectively, where S_{yx} is residual variance because of regression and b is the slope mean of the linear regression curves.

2.5.2. Accuracy and Precision

Accuracy and precision measurements are carried out at three concentrations: low, medium, and high concentrations in six replicates for the LLOQ and QC samples. Intra-day and inter-day accuracy and precision evaluations were carried out. The precision test was carried out to observe the relative standard deviation (RSD) of the responses of all samples, while the accuracy test was carried out by determining the relative error (RE). The RSD and RE values were set to be 15% for each replication of the sample [15,18].

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203 **2.5.3. Carry-over and dilution integrity**

204 Evaluation of carry-over was accomplished by incorporating the QC samples at high
205 concentrations. After that, the empty solution was injected. The response of blank solution was
206 looked after, and the response obtained should not be more than 20% of the sample solution at a
207 concentration of LLOQ [21].

208 In this study, all samples were prepared at a concentration 250 µg/mL for each metronidazole. The
209 solutions were dissolved 5 and 10 times with porcine eye liquid. Accuracy and precision were
210 finally calculated. To evaluate the integrity of the dilution, samples are analyzed using
211 concentrations of analyte above the higher concentration of the calibration standard solution.

212
213 **2.5.4. Extraction recovery**

214 In order to measure the recovery of the extracted metronidazole from the sample matrix,
215 the values were measured for all analytes from the extracted QC samples, such as the LLOQ, low,
216 medium and high concentrations. The exact concentration of samples prepared in the mobile phase
217 will be used.

218
219 **2.5.5. Stability studies**

220 Metronidazole stability studies were performed with porcine eye corneal fluid under
221 different storage and treatment conditions. Within 48 hours, an autosampler was carried out to
222 evaluate the stability of all analyte solutions. The bench-top stability evaluation was carried out at
223 room temperature for 24 hours, while the long-term stability evaluation was carried out at -20 ° C
224 for 2 weeks. Evaluation of freeze-thaw stability was carried out in three cycles with a storage
225 temperature of -20 ° C. Each response obtained was then compared with the initial response of
226 each solution.

227
228 **2.6 Application of validated HPLC method to assess ocular kinetics of metronidazole from**
229 **thermosensitive gel formulation in corneal tissue**

230 **2.6.1 Thermosensitive in situ ocular gel optimization**

231 Different thermosensitive formulation containing metronidazole were prepared using
232 Pluronic® F127 (PF127), Pluronic® F88 (PF88), and benzalkonium chloride. In this formulation,

gelling agent was used at different concentrations (**Table S3**). The responses to be examined were physical characteristics of the ocular gel which were gelation temperature and viscosity.

2.6.2 Ex vivo ocular kinetics evaluation of formulated metronidazole gels in corneal tissue

A Franz-type diffusion chamber on the porcine cornea was used in the experiment to determine the ocular kinetics and drug absorption through the cornea. Immediately after sacrificing the animal, the eyes of the porcine were collected and the corneas were carefully separated to avoid damage. This aims to get the porcine's eyeballs that were still fresh; The cornea with a scleral tissue size of 2-4 mm was carefully removed, washed with cold normal saline, then stored.

The fresh cornea was then placed between the chambers in the diffusion cells. Epithelial surface faced upwards, whereas the endothelial surface faced down towards the receptor compartment. STF at pH 7.4 was filled into the receptor compartment and then stirred gently with a magnetic stirrer. Thermosensitive *in situ* gel containing metronidazole was put into the donor compartment. At predetermined times, the cornea was collected and processed using the optimized extraction method.

2.7. Statistical analysis

Data were displayed as mean \pm standard deviation (SD). Calculations of mean, SD, % RSD, and % RE were calculated using Microsoft Excel® 2016 (Microsoft Corporation, Redmond, USA). The calculation of ocular kinetic parameters (the maximum metronidazole concentration in corneal tissue (C_{max}), the time needed to achieve the maximum concentration (t_{max}), the metronidazole concentration time in the corneal tissue curve from 0 to 72 h (AUC), the mean half-life ($t_{1/2}$) of metronidazole in corneal tissue and the mean residence time (MRT)) was used by PK Solver using non-compartment pharmacokinetic analysis [22]. Curves for comparison of drug concentration and time profiles were created. Statistical data analysis with $p < 0.05$ as a significant difference was used GraphPad Prism® version 8.3.0 (GraphPad Software Inc., San Diego, California).

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264 3. Result and Discussion

265 3.1 Sample preparation and analytes extraction

266 One-step protein precipitation was used in this study to extract and prepare metronidazole
267 from biological matrices. Permana et al. [23] have reported that this procedure is simple to be
268 applied and used. Any metabolite from biological matrices are removed to avoid analytical error
269 or column damage. The sample preparation and extraction method were optimized using a central
270 composite experimental design. As seen in **Table S4.**, two parameters, namely extraction
271 efficiency and evaporation time, were observed in this optimization process. The results showed
272 that extraction efficiency and evaporation time in three parameters fitted to the quadratic model
273 and the value of F for the efficiency of extraction and evaporation time were determined
274 respectively 10.64 and 1162.7878.

275 Extraction efficiency and evaporation time was found to be significantly affected (p
276 <0.001) this optimizing, and p -values represent it was <0.00 . **Figure 2** depicts a representative
277 three-dimensional graph showing the response of the selected factors to the extraction efficiency
278 and evaporation time. The model indicated that the extraction performance was directly
279 proportional to the volume of methanol, vortex time, and sonication time. The high extraction
280 efficiency resulted from increasing the amount of methanol volume, vortex time, and sonication
281 time in the extraction method resulting in higher extraction efficiency.

282 Finally, according to the CCD analysis, the methanol volume of 525 ml, vortex time of 15
283 minutes, and 10.091 minutes of sonication time were recommended for the extraction method to
284 obtain the optimum extraction efficiency evaporation time (**Table S5**).
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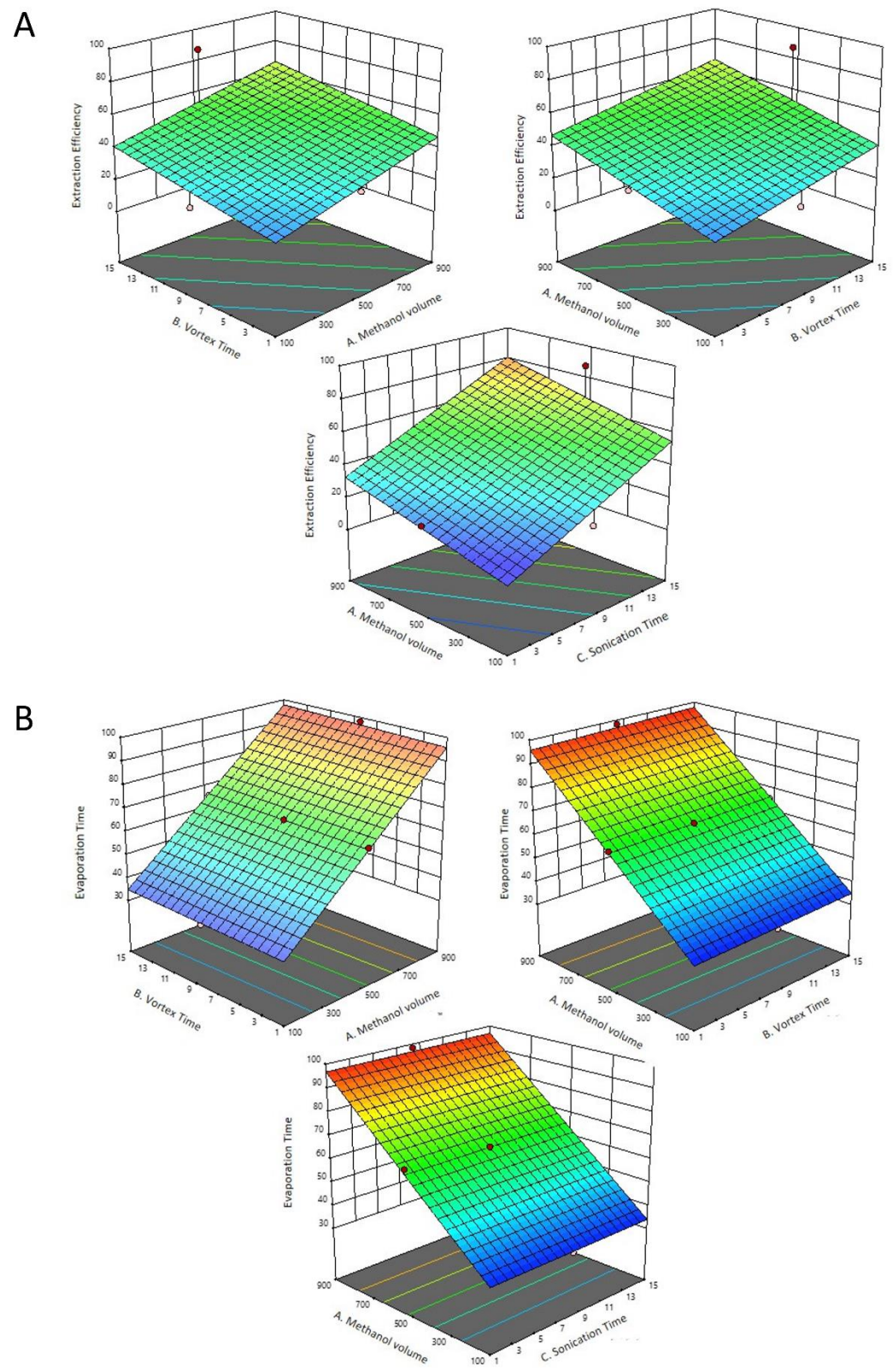


Figure 2. Illustrations of representative response surface plots illustrating the impact of the selected factors on the :
A. Extraction Efficiency; B. Evaporation time.

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3.2 Instrumentation and optimization of HPLC–UV conditions

The RP-HPLC isocratic process was used in this study. **Table S6** represented the overview result of the response surface analysis. The aim of this process is to optimize the mobile phase conditions including the concentration of acetonitrile, pH, and flow rate. **Figure 3** shows HPLC chromatograms of porcine corneal tissue fluid with and without metronidazole at a retention time of 7.32 minutes, analyzed at 313 nm. The C18 column demonstrated improved column efficiency and analyte elution with good resolution, tailing factor, and theoretical plate count. The entire separation of analytes was done by reverse C18 column due to its flexibility and suitability in analyzing and separating metronidazole [24].

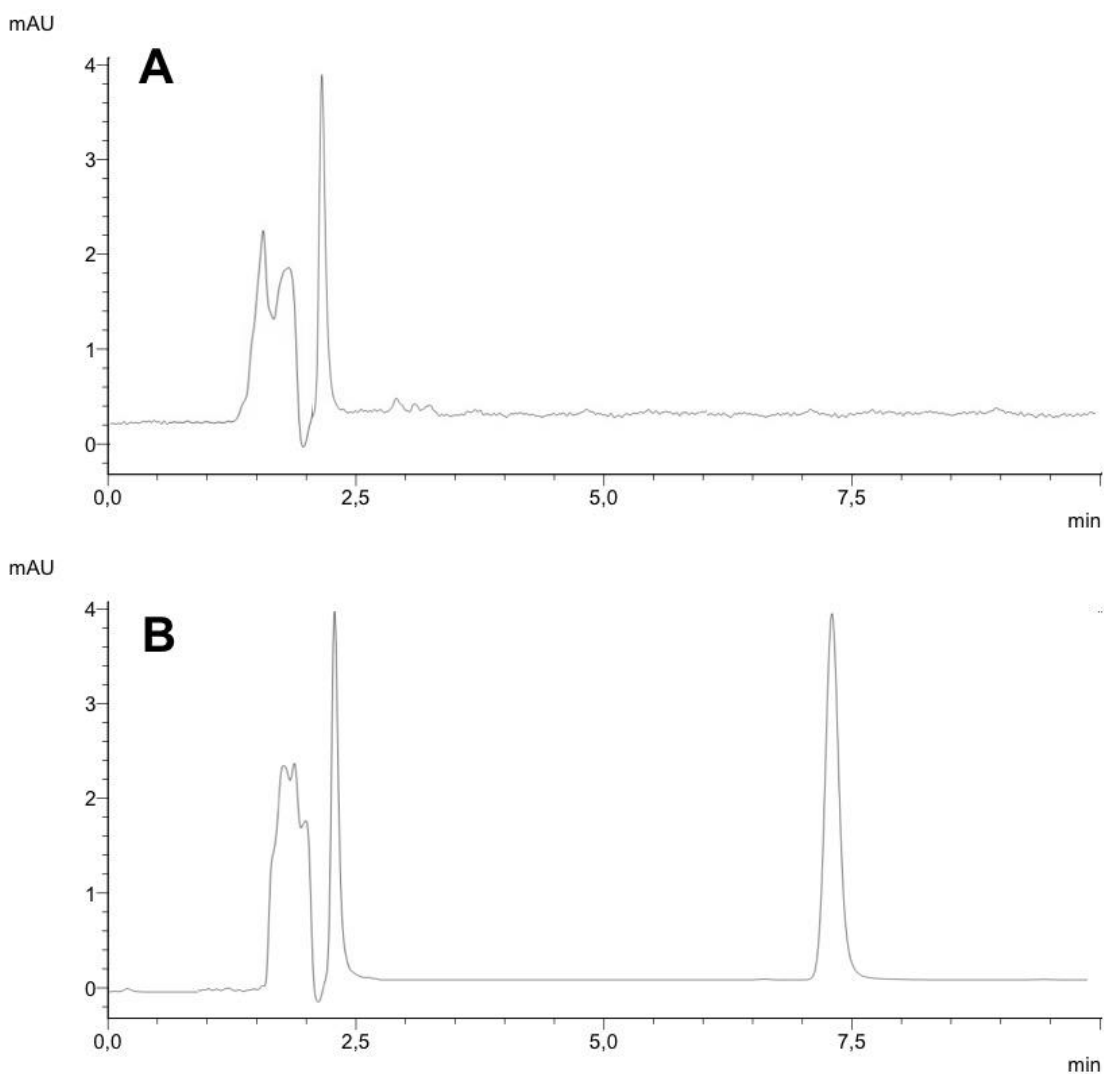


Figure 3. Representative HPLC-UV chromatograms of blank porcine eye corneal tissue fluid (A) and metronidazole with porcine eye corneal tissue fluid (B)

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4 302 The optimization process was carried out by observing effects of the theoretical plate,
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6 303 tailing factors, and retention time fitted in the quadratic model. Our analysis revealed that all of
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8 304 these parameters gave p-values of less than 0.001 when compared using the F-values from each of
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10 305 the parameters. The results showed that the F value for tailings factor, theoretical plate, and
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12 306 retention time were 15.65, 10.97, and 61.33, respectively. Therefore, we are confident that all of
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14 307 these factors were important to the optimisation process. The effect of the selected factors on
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16 308 retention time, tailings factor, and theoretical plates is shown in **Figures 4** in the form of a
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18 309 representative 3D graph. The graph shows that the combination of acetonitrile concentration, pH
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20 310 and flow rate is directly proportional to the tailings factor, theoretical plate and retention time.
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22 311 The mobile phase pH of an ionizable analyte has a significant impact on the retention activity of
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24 312 the analyte. It can be said that the pH of the mobile phase is one of the critical parameters and
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26 313 needs to be considered during the development of the method. One of them is when determining
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28 314 the pH value to achieve the desired separation. Problems in liquid chromatography often occur
29
30 315 when pH of the mobile phase is close to or equal to the pKa of the compound being analyzed,
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32 316 which is indicated by a prominent peak. Process accuracy can also be reduced by a broad peak
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34 317 accompanied by a long tail [25]. Optimization of the mobile phase can be done with this method
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36 318 by selecting the pH of the mobile phase which is one unit lower than the pKa of the compound
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38 319 under investigation [23]. In this analysis, an acetate buffer at a concentration of 20 mM was used.
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40 320 The recommended results under HPLC-UV conditions to obtain optimal tailings factor, theoretical
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42 321 plates, and retention time using software are acetonitrile concentration of 21,000 %, pH 4.505, and
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44 322 recommended flow rate of 1.020 ml/min (**Table S7**).

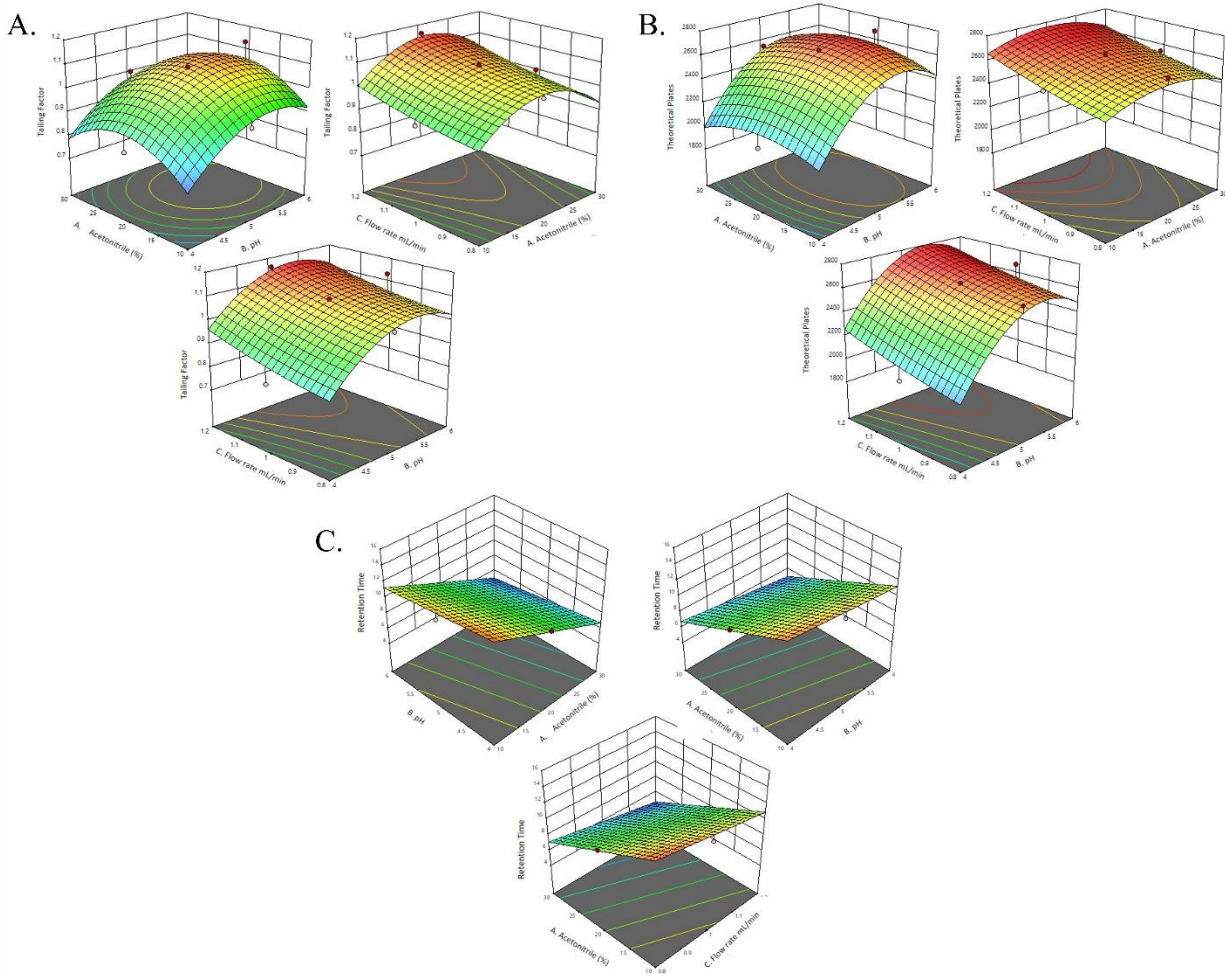


Figure 4. Illustrations of representative response surface plots illustrating the impact of the selected parameters on :
 A. Tailing factor; B. Theoretical plates and retention time; C. Retention time

3.3 Analytical method validation

3.3.1 Linearity, LOD and LLOQ

The results of the linearity of the methods, LOD, and LLOQ are shown in **Table 1**. This method is known to obtain linear values ($R = 0.999$) at concentrations ranging from 0.01 to 10 $\mu\text{g/ml}$. Excellent sensitivity was also shown by the LOD and LLOQ values as we found that metronidazole can be detected at relatively low concentration.

3.3.2 Accuracy and precision

Intra and inter-day measurements were performed to assess the precision and accuracy of this method. Metronidazole was tested on three different days as a method of evaluating accuracy and

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4 338 precision between days. Meanwhile, metronidazole measured on the same day with three
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6 339 repetitions as part of the intra-day evaluation. Based on the research, it is known that the method
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8 340 of measuring metronidazole concentrations in intra-day and inter-day measurements with good
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10 341 accuracy is at concentrations between 0.08 to 7.5 µg/mL as indicated by the %RSD value of not
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12 342 more than ± 15% (**Table 1**). In addition, this method is also considered to have good precision,
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14 343 indicated by the %RSD which decreases between 2.16 and 14.39% at the exact concentration
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16 344 measurements as above. It meets the criteria for precision measurement since it did not exceed ±
17 345 15% of the %RSD limit (**Table 1**).
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20 21 347 **3.3.3 Carry-over and dilution integrity**

22 348 Evaluation of the carry-over effect was carried out to observe the possibility of
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24 349 metronidazole signaling in the subsequent measurement of the blank solution by injecting high
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26 350 concentrations of metronidazole into the HPLC column. The tested blank solution has not more
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28 351 than 20% LLOQ in the corresponding retention time of metronidazole. The result obtained in this
29
30 352 experiment was that metronidazole was not detected in the sequence of blank solutions. This
31
32 353 indicated the absence of carry-over effects in the HPLC profile.

33 354 The dilution integrity was checked by evaluating the consistency of the concentration of
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35 355 metronidazole after the solution was diluted 5 and 10 times lower than the concentrated solution
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37 356 of metronidazole. The results of the metronidazole dilution, when analyzed using the method we
38
39 357 developed, showed recoveries between $98.21 \pm 5.19\%$ and $102.01 \pm 9.31\%$ with a precision of
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41 358 4.14%-7.42%. Based on the standard satisfaction range of accuracy (85 - 115%) and precision (±
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43 359 15%), it can be considered that the results showed excellent dilution integrity.
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45 360

46 361 **3.3.4 Recovery of Extraction**

47 362 Evaluation of the extraction recovery of porcine eye fluid and tissue was carried out by
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49 363 adding fluid at three different concentrations: low (0.08 and 0.15 µg/mL), medium (3.5 µg/mL),
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51 364 and high (7.5 µg/mL). In **Table 1**, it can be seen that the spiked sample recoveries were between
52
53 365 $94.19 \pm 8.76\%$ and $96.51 \pm 7.84\%$ with a range of %RSD values from 8.12 to 9.80%. These results
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55 366 of the %RSD value is below ±15% of the RSD, hence it is considered that the method is precise
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57 367 and consistent for the determination of metronidazole concentrations from porcine eye fluid.
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369 **3.3.5 Stability studies**

370 **Table 1** shows that metronidazole was stable under all storage conditions when added to
371 swine eye fluid. In addition, all concentration levels (low, medium, and high) showed values that
372 were acceptable to the ICH standard for stability validation [26] which were indicated by
373 recoveries values above 95% with an SD percentage of not more than 15%. Based on the literature
374 searched, there were no publications regarding the stability of metronidazole in porcine eye fluid.
375 However, there have been studies regarding the stability of metronidazole in human plasma under
376 storage conditions similar to those carried out in this study [27].

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Table 1. The results of the HPLC validation of metronidazole (n=6)

Linearity, LOD and LLOQ values				
Slope	y-intercept	R	LOD (µg/mL)	LLOQ (µg/mL)
3762.3	32.796	0.999	0.05	0.08
Intra-day Precision and Accuracy				
Replication	Concentration added (µg/mL)	Concentration found (µg/mL) ± SD	Precision (%RSD)	Accuracy (%RE)
1	0.08	0.073 ± 0.004	5.48	-8.75
	0.15	0.14 ± 0.003	2.16	-7.33
	3.5	3.57 ± 0.21	5.88	2.00
	7.5	7.63 ± 0.54	7.08	1.73
2	0.08	0.082 ± 0.003	3.66	2.50
	0.15	0.15 ± 0.021	13.64	2.67
	3.5	3.87 ± 0.37	9.56	10.57
	7.5	7.82 ± 0.69	8.82	4.27
3	0.08	0.076 ± 0.006	7.89	-5.00
	0.15	0.13 ± 0.015	11.36	-12.00
	3.5	3.94 ± 0.42	10.66	12.57
	7.5	7.43 ± 0.84	11.31	-0.93
Inter-day Precision and Accuracy				
Day	Concentration added (µg/mL)	Concentration found (µg/mL) ± SD	Precision (%RSD)	Accuracy (%RE)
1	0.08	0.076 ± 0.005	6.58	-5.00
	0.15	0.13 ± 0.019	14.39	-12.00
	3.5	3.84 ± 0.32	8.33	9.71
	7.5	7.66 ± 0.63	8.22	2.13
2	0.08	0.085 ± 0.006	7.06	6.25
	0.15	0.17 ± 0.021	12.43	12.67
	3.5	3.39 ± 0.43	12.68	-3.14
	7.5	7.65 ± 0.84	10.98	2.00
3	0.08	0.084 ± 0.004	4.76	5.00
	0.15	0.13 ± 0.012	9.16	-12.67
	3.5	3.29 ± 0.41	12.46	-6.00
	7.5	7.59 ± 0.54	7.11	1.20
Extraction recoveries				
Concentration added (µg/mL)		% Extraction Recovery ± SD	% RSD	
0.08		94.19 ± 8.76	9.30	
0.15		96.51 ± 7.84	8.12	
3.5		92.01 ± 9.02	9.80	
7.5		93.93 ± 8.89	9.46	
% Stability recoveries (mean ± SD)				
Concentration added (µg/mL)	Autosampler (48 h)	Bench-top (24 h)	Long-term (2 weeks)	Freeze-thaw (3 cycles)
0.08	98.31 ± 8.52	96.95 ± 9.04	103.21 ± 5.42	99.18 ± 8.32
0.15	101.02 ± 7.43	98.72 ± 6.03	97.64 ± 9.51	98.13 ± 8.43
3.5	99.43 ± 8.03	99.31 ± 9.43	98.39 ± 8.05	100.92 ± 7.94
7.5	96.53 ± 6.05	100.93 ± 5.65	99.53 ± 6.99	98.53 ± 9.91

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3.4 Physical properties of the formulated gels and evaluation of their ocular kinetics

3.4.1 Gelation temperature and viscosity of the formulated in-situ gels

Factors such as gelation temperature and viscosity, particularly at different conditions, are some of the most important aspects of studying thermosensitive gel preparations. Hence, we assessed these properties and compared all four formulations to see the influence of Pluronic F127 and F88 in affecting the physical characteristics of the gels. Since the eye temperature ranges from 33.5 to 35.5 [28], our goal is to formulate a thermosensitive metronidazole gel that forms a gel around these points.

In the results showing the gelation temperature (**Figure 5.IA**), it was found that all preparations formed gel at different temperatures ($p < 0.05$). Formulations A and B formed gels above body temperature while formulation C showed gelation at around 34.87 ± 3.12 °C. Formulation D, which contains Pluronic F127 alone (20%), formed gels even lower at approximately 23.64 ± 2.19 °C. The data obtained in this experiment indicated that Pluronic F88 as a combination of the gelling agent is required to obtain a suitable gelation temperature for eye applications. This finding is also in line with the previous report stating that a combination of longer hydrophobic chain poloxamers such as Pluronic F127 with more hydrophilic co-polymers is essential to the formation of gelling state at the desired temperature [9,29]. The interactions of Pluronic F127 with the other materials such as polyethylene glycol (PEG), polyvinylpyrrolidone (PVP), polyvinyl alcohol (PVA), methylcellulose (MC), and hydroxypropyl methylcellulose (HPMC) have also been demonstrated as an important factor in order to control the gelation temperature of the formulated ophthalmic sol-gel preparation [30].

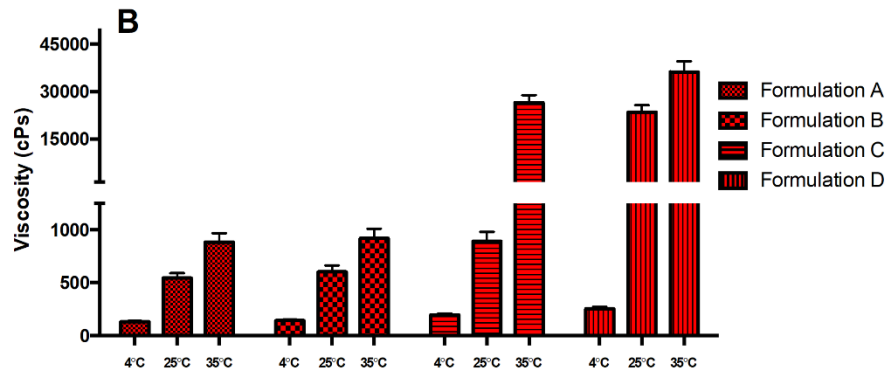
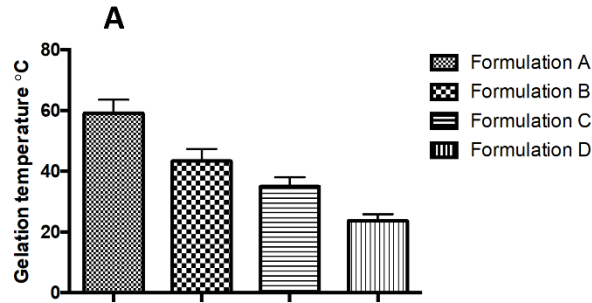
In terms of viscosity, a further investigation on the influence of Pluronic F127 and F88 toward the rheology of formulated gels also provides insight into the importance of this combination on the physical properties of the gels upon application in eye or storage. As seen in the **Figure 5.IB**, the viscosity of the gels increased as the temperature elevated. For instance, the viscosity of formulation A and B at 4 °C was 131 ± 9.32 cPs and 143 ± 8.54 cPs, respectively. When the gels are tested at room temperature, the viscosity increases, but the gelling state has not been acquired. Consistent with gelation temperatures, the viscosity of Formulation C increased significantly ($p < 0.05$) up to 26483 ± 2409 cPs when applied at eye temperature. In addition, this formulation did not form gel upon storage at 4 and 25 °C which is considered beneficial for storage conditions.

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4 414 On the other hand, Formulation D was already in the gel form when temperature reached
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6 415 around 25 °C, indicated by its viscosity (up to 23498 ± 2192 cPs) and even increased to around
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8 416 36218 ± 3381 cPs at around eye temperature. No formulation was observed to form gel at 4 °C.
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10 417 Based on these results, we agree that combination of Pluronic F127 and F88 used in formulation
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12 418 C is the most suitable mixture of these co-polymers to obtain a thermosensitive gel for ocular
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14 419 administration. However, we are also aware that this experiment is limited to the shorter time of
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16 420 storage and hence a thoroughly designed stability studies should be carried out to establish effects
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18 421 of more prolonged or even extreme storage conditions to the formulated preparations.

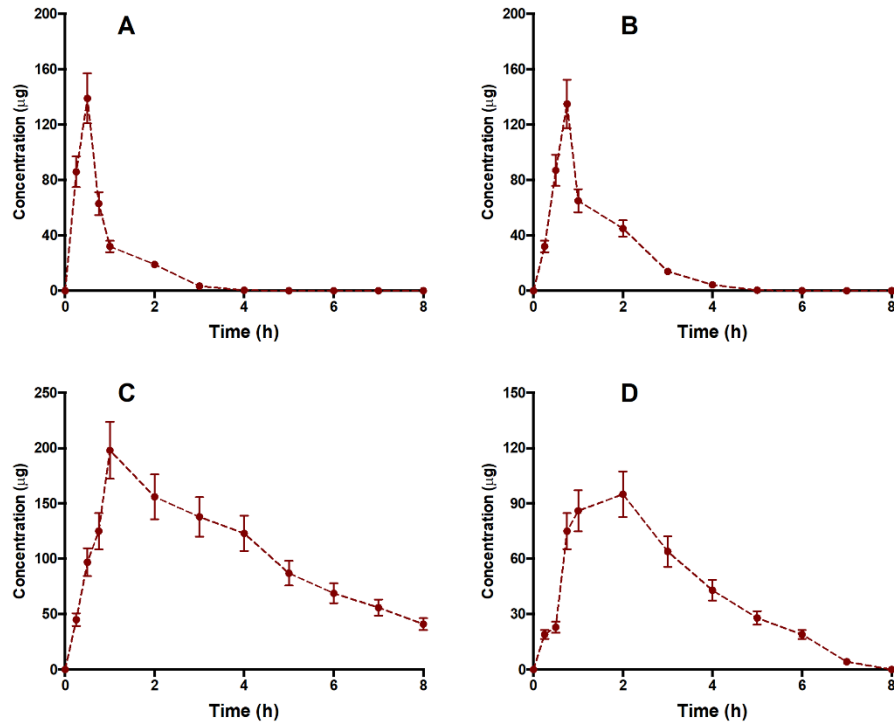
19 422 Pluronic F127 has longer hydrophobic poly(propylene oxide) (PPO) blocks compared to
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21 423 its hydrophilic poly(ethylene oxide) (PEO) blocks. In contrast, Pluronic F88 has 80% PEO relative
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23 424 to the other block chains, making this co-polymer more hydrophilic than Pluronic F127.
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25 425 Hydrophobic PPO blocks are responsible for lowering the gelation temperature while hydrophilic
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27 426 PEO blocks, otherwise, elevate the temperature [31,32]. A careful NMR study revealed that
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29 427 dehydration of PPO-PEO micelles in the solution is the key for the gelation of these co-polymers
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31 428 when applied at the specific temperature [33].

32 429 Although our findings mainly suggested that the use of Pluronic F127 and F88 is important
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34 430 in the solution-to-gel formation, it is interesting to point out that other copolymers have also been
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36 431 long utilized. For instance, in the formulation of Azithromycin thermosensitive gel, 20-22% of
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38 432 Poloxamer 404 which contain hydrophobic PPO blocks were incorporated with 5% of Poloxamer
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40 433 188 and 3-4% Carbopol 974P NF in order to obtain suitable gelation temperature of the ophthalmic
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42 434 application [34]. Alkholief, M. et.al (2010) also demonstrated this effect using a similar gel base
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44 435 in which the poloxamer and carbopol ratio was the factors that determine the slight changes in the
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46 436 gelation temperature [35]. Another example of applicable copolymers is the use of poly-(DL-lactic
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48 437 acid-co-glycolic acid) (PLGA)–polyethylene glycol (PEG)–PLGA as a thermosensitive gel base to
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50 438 deliver drugs as an ophthalmic preparations [36]. All of these evidences again supported nature of
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52 439 these polymer combinations where longer hydrophobic blocks copolymers interact with other
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54 440 materials to obtain desired properties of the gel bases. Therefore, our study also confirmed that
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56 441 physical characteristics such as gelation temperature and viscosity of thermosensitive in-situ gels
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58 442 prepared using block co-polymers depend on the influence of hydrophobic and hydrophilic blocks
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60 443 from the co-polymers.
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I.



II.



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Figure 5. I. Overall physical characteristic evaluation of thermosensitive gel preparations: (A) gelation temperature (n=3) and (B) viscosity of formulation A-D measured at 4, 25 and 35 °C (n=3); **II.** Ocular kinetic study of metronidazole thermosensitive gels showing concentration of metronidazole (μg) in corneal matrix over the measured time (hours). A-D correspond to formulation A-D which contain various types of Pluronic F127 and F88 combinations.

3.4.2 *Ex vivo ocular kinetics evaluation of formulated metronidazole gels in corneal tissue*

The validated method obtained in this study was then applied in studying the ocular kinetic of the formulated metronidazole gels. The kinetic profiles were obtained by evaluating the concentration of metronidazole from each formulated preparation in the corneal matrix. The results showing the summary of the kinetics properties of these formulations was given in **Table 2**. As indicated by the data, formulation C revealed the most significant AUC value meaning the metronidazole in porcine corneal availability is achieved better than the other formulations. It also showed a significantly higher C_{max} ($p < 0.05$) which was reached at approximately 1 hour after administration.

Meanwhile, this formula's half-life ($T_{1/2}$) was 2.54 ± 0.31 hours, a specific resident time of metronidazole in the examined compartment. Overall, metronidazole concentrations from formulation A and B were not detected at 5 hours after administration while formulation C and D can extent the drug release longer (**Figure 5.II**). It is also interesting to note that formulation A which contains 5% of Pluronic F127 and 15 % of Pluronic F88 reached the maximum concentration of 110.81 ± 9.32 $\mu\text{g/ml}$ in approximately 30 minutes after application and the longest time to reach maximum concentration was achieved by formulation D consisting of 20% of Pluronic F127 and 0% Pluronic F88. The data indicate correlation between the concentration of Pluronic combination (F127 and F88) and the availability of metronidazole in the cornea. Increasing the concentration of Pluronic F127 in the formulation A-D seems to cause the T_{max} value to be obtained at a longer time. However, there is an influence of Pluronic 127 combined with F88 in enhancing the peak corneal concentration, AUC and MRT of metronidazole since the half-life of formulation D which contains no Pluronic F88 cannot be solely improved by simply increasing Pluronic F127 concentration. Therefore, the data presented in this study is in line with our hypothesis that the combination of these two poloxamers is required in such preparations to obtain better kinetic outcomes of metronidazole.

Table 2. *Ex vivo* ocular kinetic parameters of metronidazole thermosensitive *in-situ* gels (n=3).

Parameters	Formulation A	Formulation B	Formulation C	Formulation D
C _{max} (µg)	110.81 ± 9.32	89.08 ± 8.71	171.72 ± 18.21	30.07 ± 4.31
T _{max} (h)	0.5	0.75	1	2
AUC _{0-t} (µg.h)	104.83 ± 10.21	189.59 ± 19.21	843.85 ± 90.29	37.83 ± 4.32
AUC _{0-INF} (µg.h)	104.83 ± 11.02	191.28 ± 20.12	991.36 ± 91.21	38.04 ± 3.92
T _{1/2} (h)	0.25 ± 0.02	0.78 ± 0.08	2.54 ± 0.31	0.38 ± 0.05
MRT (h)	0.69 ± 0.07	1.62 ± 0.17	4.56 ± 0.43	0.93 ± 0.12

The effect of poloxamer matrices in enhancing bioavailability of metronidazole eye preparations has not been widely available, but some evidence shows that Poloxamer-based gel is useful in improving ocular drug delivery of other drugs. Our previous report observed that gels developed using the combination of Pluronic F127 and F68 enhance the ocular kinetic of Itraconazole in an optimized thermosensitive gel preparation whether it is applied in an infected or a normal eye model [9]. Pluronic F127 with other poloxamers is also known to improve the availability of other incorporated drugs [37]. In terms of metronidazole delivery into eye tissue, Vanderbilj [6] reported that metronidazole gel showed significant diffusion rate in human and rabbit eyes compared to the eye solution. Further investigations also revealed that trans-corneal diffusion of metronidazole in human and rabbit eyes is not affected by the presence of chemical preservatives such as benzalkonium chloride [38]. In contributing to the previous knowledge available, the experiment carried out in this study provides a new insight on the relationship between poloxamer based thermosensitive gels and the kinetics of metronidazole in the eye tissue. However, it is beyond our scope to evaluate the kinetic profiles of these formulations in human or animal eye models even though factors such as tissue temperature and physiological conditions highly influence this type of pharmaceutical preparation. Therefore, we suggested that further research is carried out in addressing whether these factors are important to establish excellent kinetic profiles of metronidazole in Pluronic based thermosensitive gels.

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507 4. Conclusions

508 The development of a validation method using this new high performance liquid
509 chromatography (HPLC-UV) method was established. The new approach developed in this study
510 in which metronidazole concentrations were measured after *ex vivo* administration in porcine
511 cornea, had high precision and accuracy, simplicity, and high sensitivity and selectivity for use in
512 therapeutic drug control research and ocular kinetics evaluation.

513 As our findings suggested, the formulation of thermosensitive gels represented in this study
514 revealed influences of PF127 and PF88 combination to produce gels with an excellent gelation
515 temperature and viscosity and their ocular kinetic properties. The method we developed here was
516 also applicable in examining the concentration of metronidazole in the formulated thermosensitive
517 in-situ gel preparations. However, further research is required to fully understand whether this
518 analysis method can also be implemented in studying the drug administration under pathological
519 conditions.

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Declaration of interests

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

The authors declare the following financial interests/personal relationships which may be considered as potential competing interests:

Author Contribution Statement

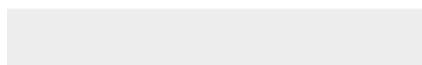
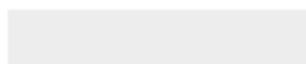
Nur Asma: Conceptualization, Methodology, Writing - Original Draft, Review & Editing;
Nurul Muhlisah Maddeppungeng: Methodology, Writing - Original Draft, Review & Editing;
Muhammad Raihan: Writing - Original Draft, Review & Editing; **Arini Putri Erdiana:** Methodology, Investigation, Data Curation; **Achmad Himawan:** Data Curation, Review & Editing, Validation, Supervision; **Andi Dian Permana:** Conceptualization, Review & Editing Project Administration, Funding Acquisition, Validation, Supervision.



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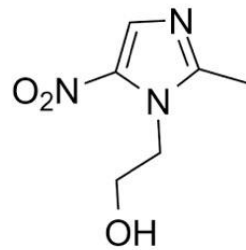
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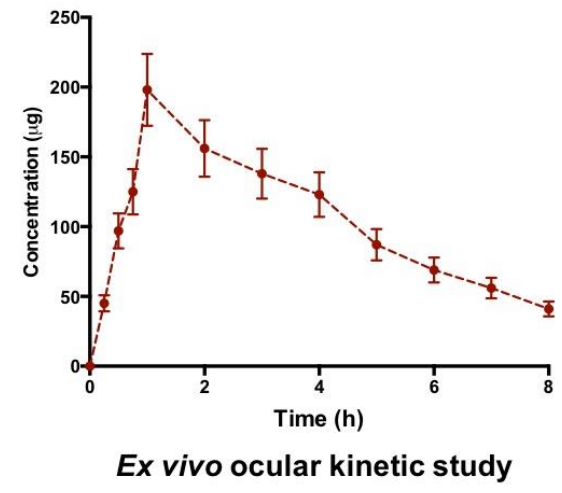




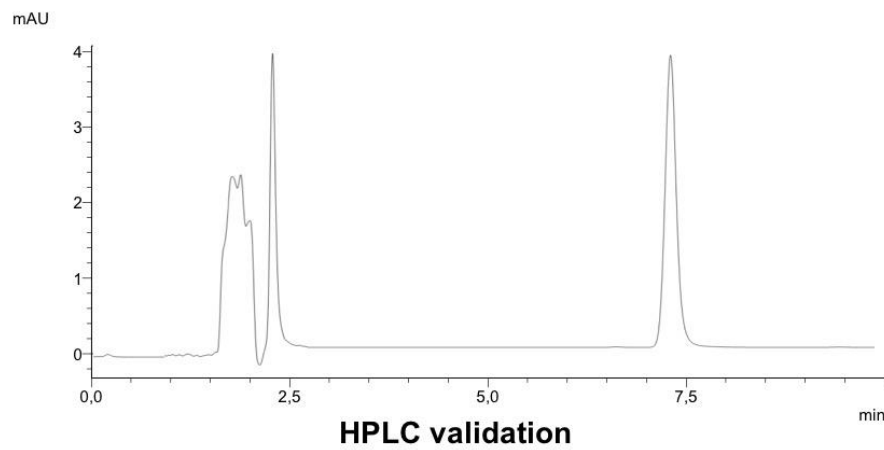
Thermosensitive *in situ* gel



Metronidazole



Ex vivo ocular kinetic study



HPLC validation

1 **New HPLC-UV analytical method for quantification of metronidazole: Application to *ex vivo***
2 **ocular kinetic assessments following the **administration** of thermosensitive ocular *in situ* gel**
3

4 Nur Asma¹, Nurul Muhlisah Maddeppungeng¹, Muhammad Raihan², Arini Putri Erdiana³,
5 Achmad Himawan³, Andi Dian Permana^{3*}
6

7 1. Department of Pharmacy, Faculty of Medicine and Health Sciences Faculty, Alauddin
8 Islamic State University, Samata Gowa, 92113, Indonesia

9 2. Department of Phytochemistry, Faculty of Pharmacy, Hasanuddin University, Makassar,
10 90245, Indonesia

11 3. Department of Pharmaceutics, Faculty of Pharmacy, Hasanuddin University, Makassar,
12 90245, Indonesia
13

14 ***Corresponding author:**

15 Andi Dian Permana

16 Faculty of Pharmacy, Hasanuddin University, Indonesia

17 Email: andi.dian.permana@farmasi.unhas.ac.id
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34 **Abstract**

35 Metronidazole eye drops have been used to treat *Acanthamoeba* keratitis. However, ophthalmic
36 preparations also have some limitations, one of which is the rapid elimination of the drug, that
37 reducing the effectiveness of the drug. Accordingly, an alternative delivery approach can be
38 applied to overcome this issue. Additionally, as one of critical steps in the formulation
39 development, analytical methods that allow the quantification of metronidazole in *ex vivo* corneal
40 permeation and deposition should also be developed. Here, we report a validated high-performance
41 liquid chromatography method (HPLC-UV) according to ICH guidelines for the measurements of
42 metronidazole concentrations following formulation of thermosensitive ocular *in situ* gel and its
43 administration in *ex vivo* porcine corneas. The development of extraction techniques and
44 optimization of HPLC conditions were optimized using analytical quality by design. Xselect™
45 CSHTM C18 HPLC column (Water, 3.0 × 150 mm, particle size 3.5 m) was used to separate all
46 analytes by isocratic elution with mobile phases of acetate buffer and acetonitrile with LLOQ value
47 of 0.08 µg/mL. The resulting method proved to be selective, precise, and accurate and was
48 successfully applied to determine ocular kinetic profiles of metronidazole from thermosensitive
49 ocular *in situ* gel in *ex vivo* porcine corneas, showing that this approach was able to improve the
50 concentration of metronidazole in the corneal tissues. We, therefore, suggested that HPLC-UV
51 approach developed in this study has the potential to be used in drug release evaluation, therapeutic
52 drug control research, ocular kinetics, and toxicological evaluation.

53 **Keywords:**

54 Metronidazole, keratitis, HPLC, thermosensitive *in situ* gel, ocular kinetic, method validation

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66 **1. Introduction**

67 Infection that presents with corneal ulcerations known as Acanthamoeba keratitis is caused
68 by *Acanthamoeba* species. It was first reported in 1973. This condition occurs commonly when
69 someone uses a contact lens washing solution prepared with non-sterile salt tablets and water [1].

70 Metronidazole is a derivative of 5-Nitroimidazole known to act as a powerful antibacterial
71 and antiprotozoal. For decades, eye preparations has become a fast growing pharmaceutical
72 technology [2]. In ophthalmology, general eye drops and topical eye preparations are the most
73 widely used preparations. It is considered the most efficient form of treating infections of the
74 foreground structures generally caused by anaerobic bacteria [3]. Acanthamoeba keratitis can be
75 treated using 0.5% metronidazole eye drops mixed with other antiprotozoal preparations [4].
76 Metronidazole eye drops have long been a formulary drug in pharmacies as an alternative to the
77 lack of a commercially available form of eye medications. In ophthalmology, preparations with
78 0.1% and 0.5% metronidazole solutions have been used to treat Acanthamoeba keratitis [5–7].

79 Topical administration of the drug is more prevalent among patients and safer than the
80 intraocular injection, but topical use of this drug has the disadvantage that the drug cannot be
81 adequately absorbed in the eye and reaches the posterior segment. As a part of trends in topical
82 formulation, thermosensitive gels have been utilized in overcoming these problems. The term
83 thermosensitive refers to its ability to form gel or solution reversibly upon at a particular
84 temperature. This can be achieved by taking advantages of unique properties of some gelling agent
85 such as N-acrylamide based co-polymers and poly(propylene oxide) (PPO)/ polyethylene oxide
86 (PEO) block co-polymers [8]. However, previous reports showed that combination of two co-
87 polymers or its interaction with other gelling agents is required to obtained a relatively precise
88 temperature for the gel to form [9–11]. To our best understanding, this is the first time the
89 technology of thermosensitive gels is applied to administer metronidazole in an ocular drug
90 delivery. Therefore, it is also an important task to assess whether the newly incorporated gel bases
91 is able to release metronidazole upon application in the eye condition.

92 Over the last few decades, many improved methods have been undertaken to find and
93 explore more effective ways of administering eye medications and treatments for various eye
94 diseases [12]. In transcorneal penetration studies, *in vitro* cell culture models have been widely
95 selected. The development of an organotypic corneal construction technique also studies the

96 bioavailability of ophthalmic drugs using primary cell cultures and immortalized cell lines. There
97 is great potential for research into corneal penetration in artificially cultivated human corneas.
98 Using a research model using cut animal corneal tissue to study drug penetration is one technique
99 with promising results, although it is necessary to consider the significant variation between
100 species [13]. One of the developments in the new *ex vivo* model is to use a porcine cornea disc. It
101 is considered to be more cost-effective for candidates for transcorneal penetrating topical therapy
102 [14].

103 Method development and validation have tremendous importance in the QC of the drug. In
104 recent years because of its importance, the development of new testing methods for drug
105 determination has received considerable attention in **determining** potency of active ingredients in
106 eye drops. Hence, HPLC is the analytical method of choice for measuring metronidazole [7]. The
107 HPLC method validation test will be conducted according to guidelines recommended by the
108 USFDA (2001) [15]. Comparison between the retention times of metronidazole detected in the
109 drug-free plasma assay and metronidazole derived from drug injection extracted from spiked
110 plasma will be investigated as a test of specificity and selectivity [7].

111 **Several previous studies related to HPLC and LC-MS/MS for the quantification of**
112 **metronidazole in various biological matrices have been carried out. A study by Silva et al (2009)**
113 **showed simple, fast, sensitive, and selective results using liquid chromatography (LC)-tandem**
114 **mass spectrometry (MS-NONA)[16]. In addition, HPLC and LC-MS/MS for metronidazole**
115 **quantification have also been performed on saliva, plasma, and gingival crevicular fluid [17].**

116 Transcorneal penetration of metronidazole using *ex vivo* porcine corneal model has never
117 been developed. The development of extraction method before having HPLC assay is essential to
118 produce maximum drug concentration. **Optimization and development** of analytical methods, also
119 **recognized** as the analytical quality by design (AQbD), are now widely applied to quality by design
120 (QbD). This concept is considered necessary since **the first time** it was first introduced by the
121 USFDA [18]. This concept is known to require less time for experimentation because it uses the
122 experimental design method (DOE) to obtain possible combinations of parameters and has also
123 been recommended in robustness testing [18,19]. Implementation **of** AQbD applications in HPLC
124 method development has been done in many studies, Rozet et al reported using AQbD approach
125 for analytical method by HPLC [20]. Prior to analyzing metronidazole with HPLC, we developed
126 an optimised method for extracting drug form matrix using various sonication time and stirring

127 time. This aimed to maximise the number of metronidazole that were measured using HPLC
128 method. The validated HPLC method will be used to assess the *ex vivo* ocular kinetics of the drug
129 after topical application to the eye.

130

131 **2. Materials and methods**

132 **2.1. Chemicals and materials**

133 Metronidazole ($\geq 99.9\%$, purity), analytical grade trifluoroacetic acid, and HPLC-grade
134 Methanol (MeOH) (Sigma-Aldrich Pte Ltd, Singapore), Xselect CSH™ C₁₈ HPLC column
135 (particle size 3.5 μm , 3, 0 \times 150 mm; Waters, Dublin, Ireland), chemical reagent (Sigma - Aldrich
136 Pte Ltd, Singapore). Other reagents were analytical grade and obtained from standard commercial
137 supplier.

138

139 **2.2. Stock Preparation, Calibration Standards and Quality Control Samples**

140 Metronidazole stock solution was prepared by dissolving 50 mg in 50 ml methanol so that
141 a concentration of 1 mg/mL was obtained. The working solutions were diluted into serial
142 concentrations for standard calibration, and quality control (QC) solutions. In the calibration of the
143 test method, a concentration series was made using the stock solution diluted with porcine eye
144 corneal tissue matrices. The final concentrations obtained ranged from 0.01 to 10 $\mu\text{g/mL}$. QC
145 solutions were made in three types of concentrations, namely 0.15 $\mu\text{g/mL}$, 3.5 $\mu\text{g/mL}$ and 7.5
146 $\mu\text{g/mL}$ for low QC, medium QC and high QC, respectively. All QC solutions were prepared in
147 porcine eye corneal tissue matrices.

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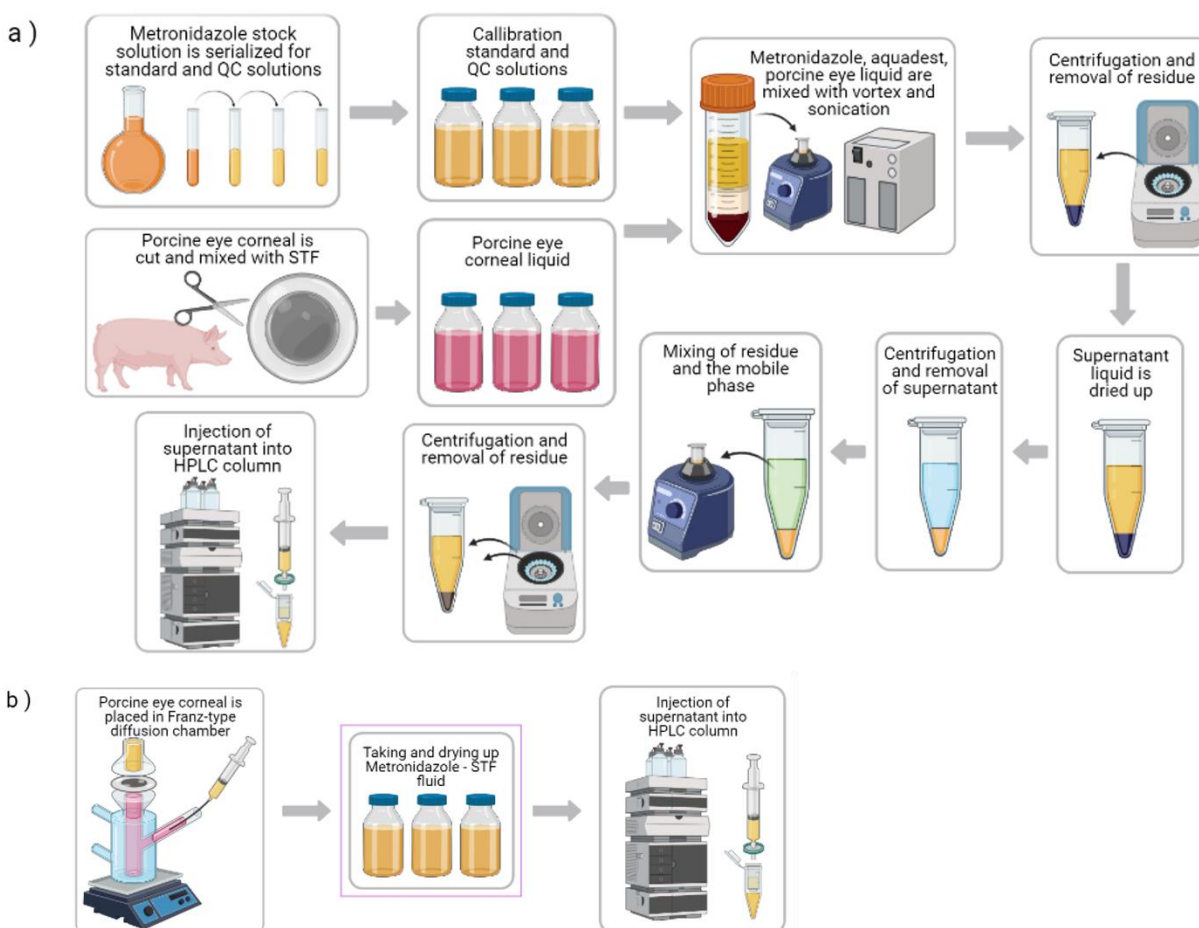
149 **2.3. Preparation and Analytes Extraction of Samples**

150 Simulated tear fluid consisting of 6.7 g NaCl, 2.0 g NaHCO₃ and 0.08
151 g CaCl₂·2H₂O was initially prepared by dissolving all components in 1
152 L deionized water (final pH of 7.4). Preparation of the sample was conducted by mixing porcine
153 eye corneal 2,5 g with 2,5 g STF (stimulated tear fluid) pH 7,4 to make porcine eye corneal fluid,
154 2 mg of metronidazole was added with 2 mL aquadest. The 100 μL of the mixture was centrifuged
155 with 900 μL porcine eye corneal fluid. The extraction volume, stirring time and sonication time
156 were evaluated. The response surface methodology to optimize sonication time, vortex time, and
157 methanol volume (Table S1) used Composite Central Design (CCD) by Design Expert Software

158 version 11 (State-Ease, Minneapolis, MN, USA). The response parameters were extraction
159 performance and fluid evaporation time.

160 The supernatant liquid was put into a small glass container and then dried up in a fume
161 hood for about 3 hours. This is done in order to obtain dried residue. The residual mixture and the
162 100 μ L mobile phase were stored in a 0.5 mL centrifuge tube. For 30 seconds, the mixture was
163 stirred and then rotated at 14,000 rpm \times g for 15 minutes. A total of 10 μ L of the treated supernatant
164 solution was injected into the HPLC column. The work steps are illustrated in **Figure 1**.

165



166

167 **Figure 1.** Illustration of the work steps

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169 **2.4. Instrumentation and Optimisation of HPLC–UV conditions**

170 Simultaneous analysis of the entire analyte applied using HPLC system (Shimadzu
171 Prominence, Shimadzu, Kyoto, Japan) equipped with PDA detector; acetonitrile and 20 mM

172 acetate buffer were utilized as the mobile phases; the separation of analytes using Xselect CSH™
173 C18 column (Waters, 3.0 × 150 mm); 3.5 μm particle size with guard cartridge.
174 CCD was used in the response surface methodology to optimize mobile phase, flow rate, mobile
175 phase pH, and acetonitrile concentration (**Table S2**). Design Expert® Software version 11 (State-
176 Ease, Minneapolis, MN, USA) was used in processing the data and performed statistical analyses.
177 Parameters recorded response were the retention time (RT), the theoretical plates and tailing
178 factors.

179

180 **2.5. Analytical method validation**

181 Based on US FDA and ICH guidelines, the developed bioanalytical method was validated
182 [15,18]. Validated parameters were precision, accuracy, linearity, selectivity, carry over, extraction
183 recovery, lower limit of quantification (LLOQ), dilution integrity, and stability.

184

185 **2.5.1. Linearity, LOD and LLOQ**

186 Linearity was measured by a calibration curve derived from a sample with a working
187 standard solution. The calibration curve was made of seven levels of concentration with three
188 separate times.

189 The limits of detection and limits of quantification were determined by the regression of
190 the obtained standard curves. LOD and LOQ were represented as $3.3 \times S_{yx}/b$ and $10.0 \times S_{yx}/b$,
191 respectively, where S_{yx} is residual variance because of regression and b is the slope mean of the
192 linear regression curves.

193

194 **2.5.2. Accuracy and Precision**

195 Accuracy and precision measurements are carried out at three concentrations: low,
196 medium, and high concentrations in six replicates for the LLOQ and QC samples. Intra-day and
197 inter-day accuracy and precision evaluations were carried out. The precision test was carried out
198 to observe the relative standard deviation (RSD) of the responses of all samples, while the accuracy
199 test was carried out by determining the relative error (RE). The RSD and RE values were set to be
200 15% for each replication of the sample [15,18].

201

202

203 **2.5.3. Carry-over and dilution integrity**

204 Evaluation of carry-over was accomplished by incorporating the QC samples at high
205 concentrations. After that, the empty solution was injected. The response of blank solution was
206 looked after, and the response obtained should not be more than 20% of the sample solution at a
207 concentration of LLOQ [21].

208 In this study, all samples were prepared at a concentration 250 µg/mL for each metronidazole. The
209 solutions were dissolved 5 and 10 times with porcine eye liquid. Accuracy and precision were
210 finally calculated. To evaluate the integrity of the dilution, samples are analyzed using
211 concentrations of analyte above the higher concentration of the calibration standard solution.

212

213 **2.5.4. Extraction recovery**

214 In order to measure the recovery of the extracted metronidazole from the sample matrix,
215 the values were measured for all analytes from the extracted QC samples, such as the LLOQ, low,
216 medium and high concentrations. The exact concentration of samples prepared in the mobile phase
217 will be used.

218

219 **2.5.5. Stability studies**

220 Metronidazole stability studies were performed with porcine eye corneal fluid under
221 different storage and treatment conditions. Within 48 hours, an autosampler was carried out to
222 evaluate the stability of all analyte solutions. The bench-top stability evaluation was carried out at
223 room temperature for 24 hours, while the long-term stability evaluation was carried out at -20 ° C
224 for 2 weeks. Evaluation of freeze-thaw stability was carried out in three cycles with a storage
225 temperature of -20 ° C. Each response obtained was then compared with the initial response of
226 each solution.

227

228 **2.6 Application of validated HPLC method to assess ocular kinetics of metronidazole from**
229 **thermosensitive gel formulation in corneal tissue**

230 **2.6.1 Thermosensitive in situ ocular gel optimization**

231 Different thermosensitive formulation containing metronidazole were prepared using
232 Pluronic® F127 (PF127), Pluronic® F88 (PF88), and benzalkonium chloride. In this formulation,

233 gelling agent was used at different concentrations (**Table S3**). The responses to be examined were
234 physical characteristics of the ocular gel which were gelation temperature and viscosity.

235

236 **2.6.2 *Ex vivo* ocular kinetics evaluation of formulated metronidazole gels in corneal tissue**

237 **A** Franz-type diffusion chamber on the porcine cornea was used in the experiment to
238 determine the ocular kinetics and drug absorption through the cornea. Immediately after sacrificing
239 the animal, the eyes of the porcine were collected and the corneas were carefully separated to avoid
240 damage. This aims to get the porcine's eyeballs that were still fresh; The cornea with a scleral
241 tissue size of 2-4 mm was carefully removed, washed with cold normal saline, then stored.

242 The **fresh** cornea was then placed between the chambers in the diffusion cells. Epithelial
243 surface faced upwards, whereas **the** endothelial surface faced down towards the receptor
244 compartment. STF at pH 7.4 was filled into the receptor compartment and then stirred gently with
245 a magnetic stirrer. Thermosensitive *in situ* gel containing metronidazole was put into the donor
246 compartment. At predetermined times, **the cornea** was collected and processed using the optimized
247 extraction method.

248

249 **2.7. Statistical analysis**

250 Data were displayed as mean \pm standard deviation (SD). Calculations of mean, SD, % RSD,
251 and % RE were calculated using Microsoft Excel® 2016 (Microsoft Corporation, Redmond,
252 USA). The calculation of ocular kinetic parameters (**the maximum metronidazole concentration in
253 corneal tissue (C_{max}), the time needed to achieve the maximum concentration (t_{max}), the
254 metronidazole concentration time in the corneal tissue curve from 0 to 72 h (AUC), the mean half-
255 life ($t_{1/2}$) of metronidazole in corneal tissue and the mean residence time (MRT))**) was used by PK
256 Solver using non-compartment pharmacokinetic analysis [22]. Curves for comparison of drug
257 concentration and time profiles were created. Statistical data analysis with $p < 0.05$ as a significant
258 difference was used GraphPad Prism® version 8.3.0 (GraphPad Software Inc., San Diego,
259 California).

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264 **3. Result and Discussion**

265 **3.1 Sample preparation and analytes extraction**

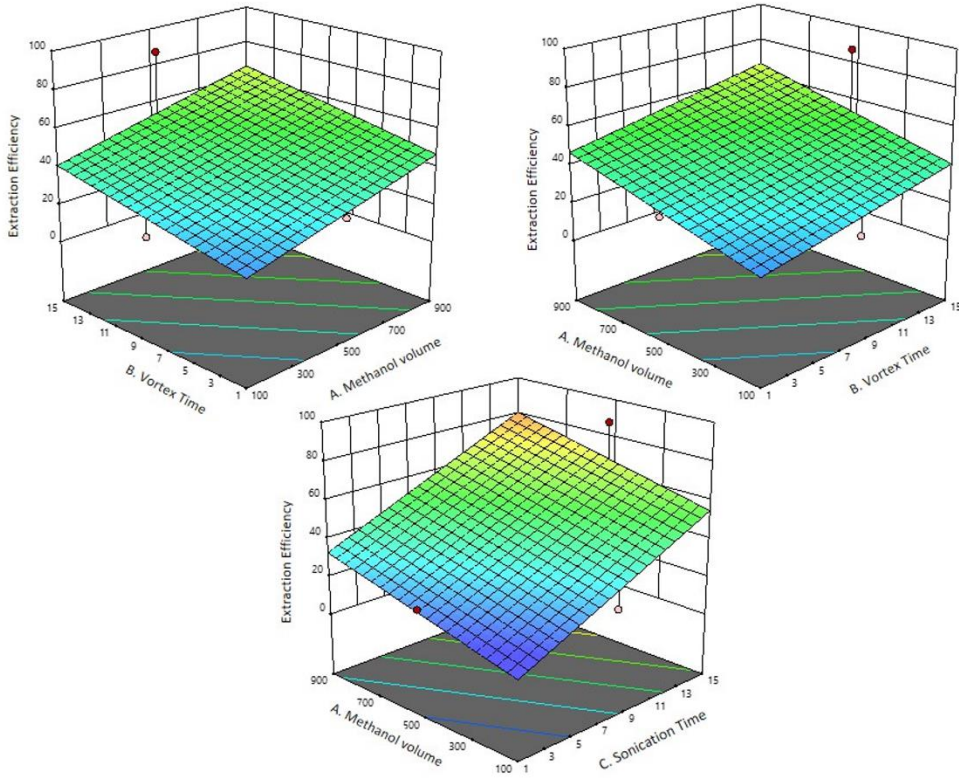
266 One-step protein precipitation was used in this study to extract and prepare metronidazole
267 from biological matrices. Permana et al. [23] have reported that this procedure is simple to be
268 applied and used. Any metabolite from biological matrices are removed to avoid analytical error
269 or column damage. The sample preparation and extraction method were optimized using a central
270 composite experimental design. As seen in **Table S4.**, two parameters, namely extraction
271 efficiency and evaporation time, were observed in this optimization process. The results showed
272 that extraction efficiency and evaporation time in three parameters fitted to the quadratic model
273 and the value of F for the efficiency of extraction and evaporation time were determined
274 respectively 10.64 and 1162.7878.

275 Extraction efficiency and evaporation time was found to be significantly affected (p
276 <0.001) this optimizing, and p -values represent it was <0.00 . **Figure 2** depicts a representative
277 three-dimensional graph showing the response of the selected factors to the extraction efficiency
278 and evaporation time. The model indicated that the extraction performance was directly
279 proportional to the volume of methanol, vortex time, and sonication time. The high extraction
280 efficiency resulted from increasing the amount of methanol volume, vortex time, and sonication
281 time in the extraction method resulting in higher extraction efficiency.

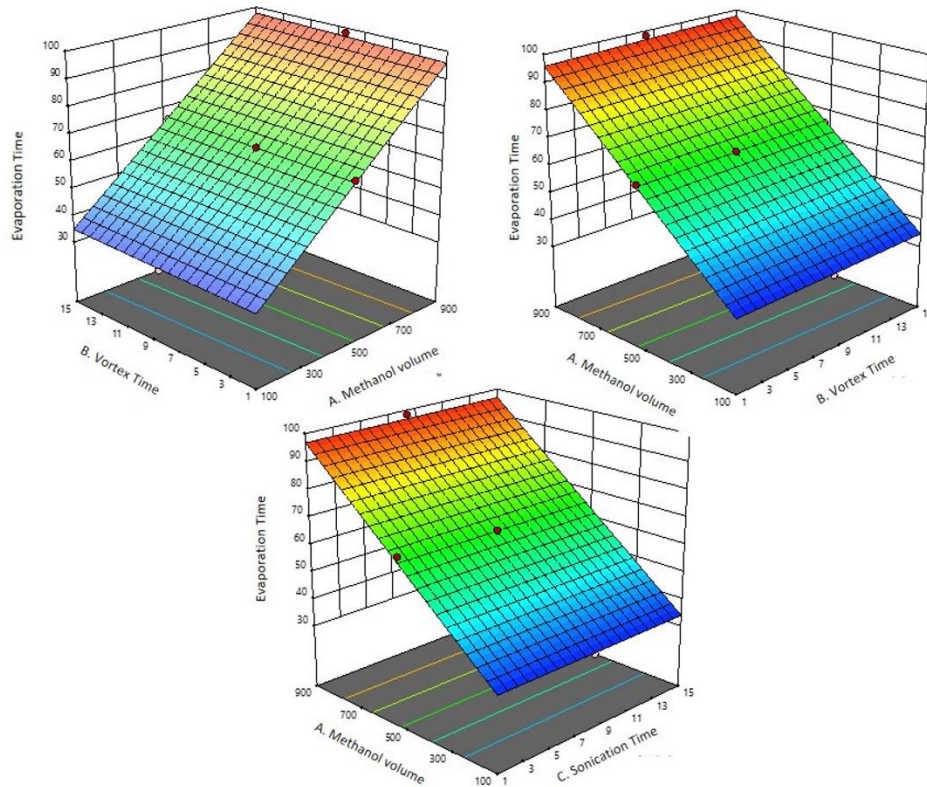
282 Finally, according to the CCD analysis, the methanol volume of 525 ml, vortex time of 15
283 minutes, and 10.091 minutes of sonication time were recommended for the extraction method to
284 obtain the optimum extraction efficiency evaporation time (**Table S5**).

285

A



B



286

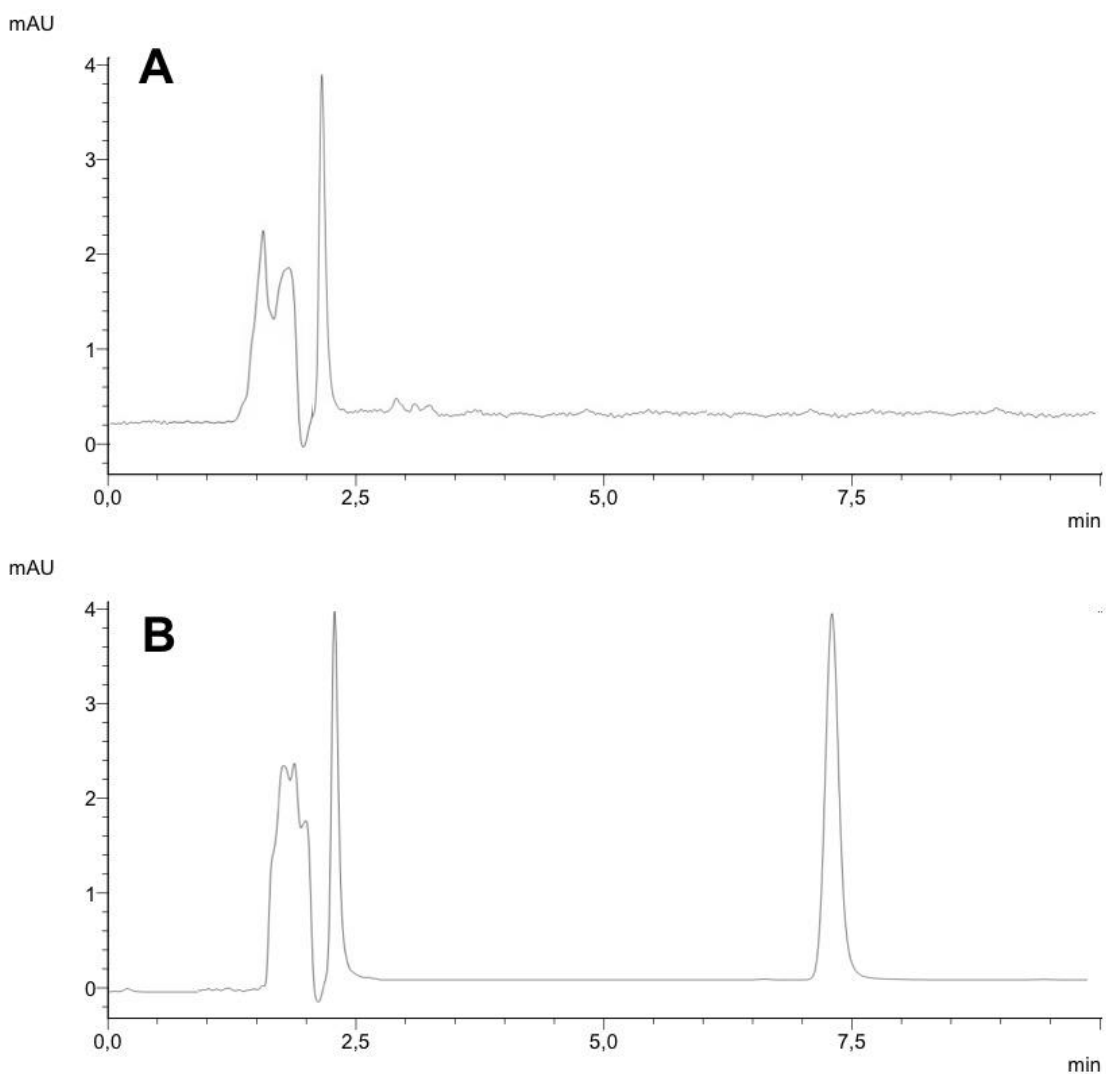
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Figure 2. Illustrations of representative response surface plots illustrating the impact of the selected factors on the :
 A. Extraction Efficiency; B. Evaporation time.

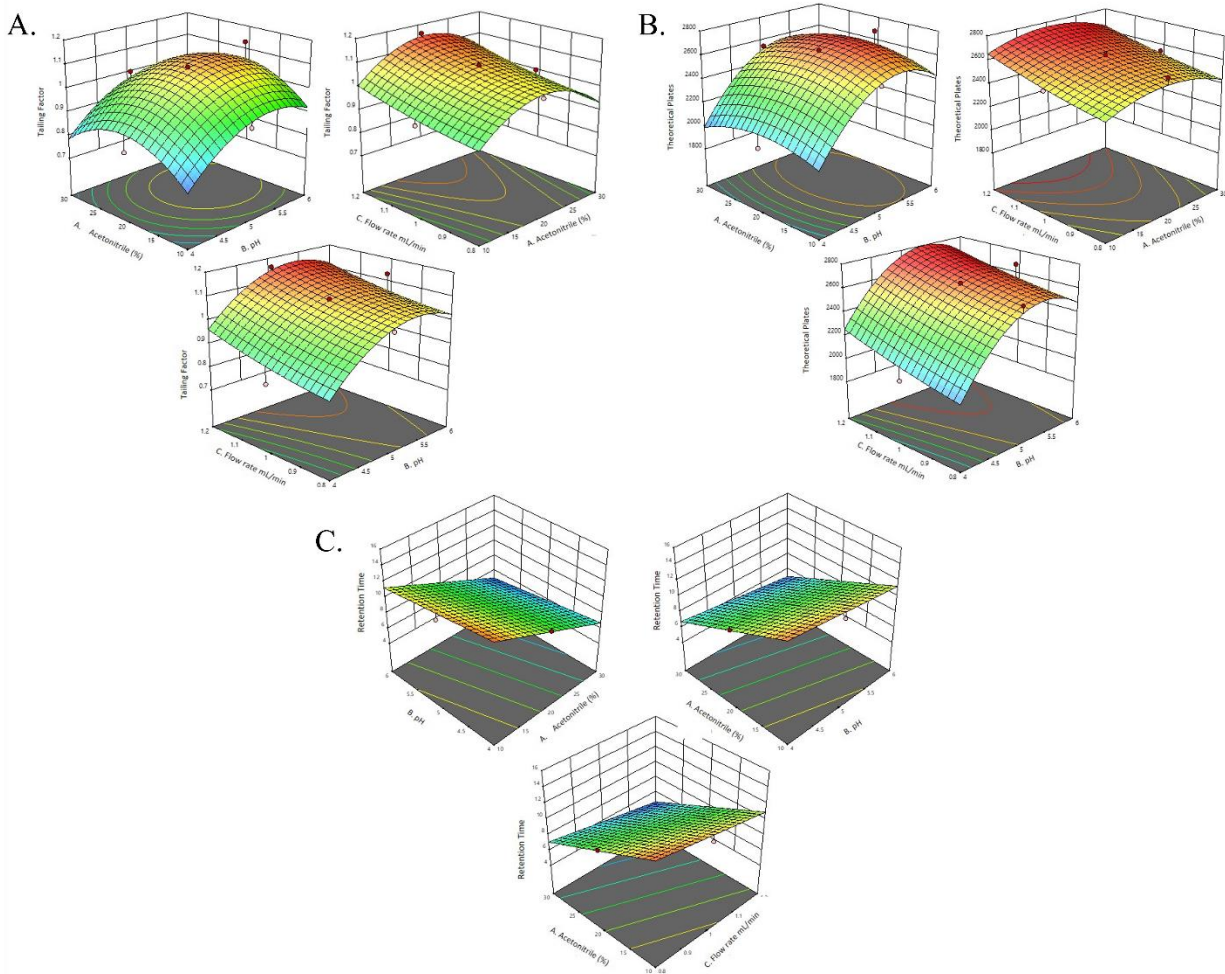
289 **3.2 Instrumentation and optimization of HPLC–UV conditions**

290 The RP-HPLC isocratic process was used in this study. **Table S6** represented the overview
291 result of the response surface analysis. The aim of this process is to optimize the mobile phase
292 conditions including the concentration of acetonitrile, pH, and flow rate. **Figure 3** shows HPLC
293 chromatograms of porcine corneal tissue fluid with and without metronidazole at a retention time
294 of 7.32 minutes, analyzed at 313 nm. The C18 column demonstrated improved column efficiency
295 and analyte elution with good resolution, tailing factor, and theoretical plate count. The entire
296 separation of analytes was done by reverse C18 column due to its flexibility and suitability in
297 analyzing and separating metronidazole [24].



298 **Figure 3.** Representative HPLC-UV chromatograms of blank porcine eye corneal tissue fluid (A) and metronidazole
299 with porcine eye corneal tissue fluid (B)
300
301

302 The optimization process was carried out by observing effects of the theoretical plate,
303 tailing factors, and retention time fitted in the quadratic model. Our analysis revealed that all of
304 these parameters gave p-values of less than 0.001 when compared using the F-values from each of
305 the parameters. The results showed that the F value for tailings factor, theoretical plate, and
306 retention time were 15.65, 10.97, and 61.33, respectively. Therefore, we are confident that all of
307 these factors were important to the optimisation process. The effect of the selected factors on
308 retention time, tailings factor, and theoretical plates is shown in **Figures 4** in the form of a
309 representative 3D graph. The graph shows that the combination of acetonitrile concentration, pH
310 and flow rate is directly proportional to the tailings factor, theoretical plate and retention time.
311 The mobile phase pH of an ionizable analyte has a significant impact on the retention activity of
312 the analyte. It can be said that the pH of the mobile phase is one of the critical parameters and
313 needs to be considered during the development of the method. One of them is when determining
314 the pH value to achieve the desired separation. Problems in liquid chromatography often occur
315 when pH of the mobile phase is close to or equal to the pKa of the compound being analyzed,
316 which is indicated by a prominent peak. Process accuracy can also be reduced by a broad peak
317 accompanied by a long tail [25]. Optimization of the mobile phase can be done with this method
318 by selecting the pH of the mobile phase which is one unit lower than the pKa of the compound
319 under investigation [23]. In this analysis, an acetate buffer at a concentration of 20 mM was used.
320 The recommended results under HPLC-UV conditions to obtain optimal tailings factor, theoretical
321 plates, and retention time using software are acetonitrile concentration of 21,000 %, pH 4.505, and
322 recommended flow rate of 1.020 ml/min (**Table S7**).



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Figure 4. Illustrations of representative response surface plots illustrating the impact of the selected parameters on :
A. Tailing factor; B. Theoretical plates and retention time; C. Retention time

328 **3.3 Analytical method validation**

329 **3.3.1 Linearity, LOD and LLOQ**

330 The results of the linearity of the methods, LOD, and LLOQ are shown in **Table 1**. This
331 method is known to obtain linear values ($R = 0.999$) at concentrations ranging from 0.01 to 10
332 $\mu\text{g/ml}$. Excellent sensitivity was also shown by the LOD and LLOQ values as we found that
333 metronidazole can be detected at relatively low concentration.

334

335 **3.3.2 Accuracy and precision**

336 Intra and inter-day measurements were performed to assess the precision and accuracy of this
337 method. Metronidazole was tested on three different days as a method of evaluating accuracy and

338 precision between days. Meanwhile, metronidazole measured on the same day with three
339 repetitions as part of the intra-day evaluation. Based on the research, it is known that the method
340 of measuring metronidazole concentrations in intra-day and inter-day measurements with good
341 accuracy is at concentrations between 0.08 to 7.5 $\mu\text{g}/\text{mL}$ as indicated by the %RSD value of not
342 more than $\pm 15\%$ (**Table 1**). In addition, this method is also considered to have good precision,
343 indicated by the %RSD which decreases between 2.16 and 14.39% at the exact concentration
344 measurements as above. It meets the criteria for precision measurement since it did not exceed \pm
345 15% of the %RSD limit (**Table 1**).

346

347 **3.3.3 Carry-over and dilution integrity**

348 Evaluation of the carry-over effect was carried out to observe the possibility of
349 metronidazole signaling in the subsequent measurement of the blank solution by injecting high
350 concentrations of metronidazole into the HPLC column. The tested blank solution has not more
351 than 20% LLOQ in the corresponding retention time of metronidazole. The result obtained in this
352 experiment was that metronidazole was not detected in the sequence of blank solutions. This
353 indicated the absence of carry-over effects in the HPLC profile.

354 The dilution integrity was checked by evaluating the consistency of the concentration of
355 metronidazole after the solution was diluted 5 and 10 times lower than the concentrated solution
356 of metronidazole. The results of the metronidazole dilution, when analyzed using the method we
357 developed, showed recoveries between $98.21 \pm 5.19\%$ and $102.01 \pm 9.31\%$ with a precision of
358 4.14%-7.42%. Based on the standard satisfaction range of accuracy (85 - 115%) and precision (\pm
359 15%), it can be considered that the results showed excellent dilution integrity.

360

361 **3.3.4 Recovery of Extraction**

362 Evaluation of the extraction recovery of porcine eye fluid and tissue was carried out by
363 adding fluid at three different concentrations: low (0.08 and 0.15 $\mu\text{g}/\text{mL}$), medium (3.5 $\mu\text{g}/\text{mL}$),
364 and high (7.5 $\mu\text{g}/\text{mL}$). In **Table 1**, it can be seen that the spiked sample recoveries were between
365 $94.19 \pm 8.76\%$ and $96.51 \pm 7.84\%$ with a range of %RSD values from 8.12 to 9.80%. These results
366 of the %RSD value is below $\pm 15\%$ of the RSD, hence it is considered that the method is precise
367 and consistent for the determination of metronidazole concentrations from porcine eye fluid.

368

369 **3.3.5 Stability studies**

370 **Table 1** shows that metronidazole was stable under all storage conditions when added to
371 swine eye fluid. In addition, all concentration levels (low, medium, and high) showed values that
372 were acceptable to the ICH standard for stability validation [26] which were indicated by
373 recoveries values above 95% with an SD percentage of not more than 15%. Based on the literature
374 searched, there were no publications regarding the stability of metronidazole in porcine eye fluid.
375 However, there have been studies regarding the stability of metronidazole in human plasma under
376 storage conditions similar to those carried out in this study [27].

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Table 1. The results of the HPLC validation of metronidazole (n=6)

Linearity, LOD and LLOQ values				
Slope	y-intercept	R	LOD (µg/mL)	LLOQ (µg/mL)
3762.3	32.796	0.999	0.05	0.08
Intra-day Precision and Accuracy				
Replication	Concentration added (µg/mL)	Concentration found (µg/mL) ± SD	Precision (%RSD)	Accuracy (%RE)
1	0.08	0.073 ± 0.004	5.48	-8.75
	0.15	0.14 ± 0.003	2.16	-7.33
	3.5	3.57 ± 0.21	5.88	2.00
	7.5	7.63 ± 0.54	7.08	1.73
2	0.08	0.082 ± 0.003	3.66	2.50
	0.15	0.15 ± 0.021	13.64	2.67
	3.5	3.87 ± 0.37	9.56	10.57
	7.5	7.82 ± 0.69	8.82	4.27
3	0.08	0.076 ± 0.006	7.89	-5.00
	0.15	0.13 ± 0.015	11.36	-12.00
	3.5	3.94 ± 0.42	10.66	12.57
	7.5	7.43 ± 0.84	11.31	-0.93
Inter-day Precision and Accuracy				
Day	Concentration added (µg/mL)	Concentration found (µg/mL) ± SD	Precision (%RSD)	Accuracy (%RE)
1	0.08	0.076 ± 0.005	6.58	-5.00
	0.15	0.13 ± 0.019	14.39	-12.00
	3.5	3.84 ± 0.32	8.33	9.71
	7.5	7.66 ± 0.63	8.22	2.13
2	0.08	0.085 ± 0.006	7.06	6.25
	0.15	0.17 ± 0.021	12.43	12.67
	3.5	3.39 ± 0.43	12.68	-3.14
	7.5	7.65 ± 0.84	10.98	2.00
3	0.08	0.084 ± 0.004	4.76	5.00
	0.15	0.13 ± 0.012	9.16	-12.67
	3.5	3.29 ± 0.41	12.46	-6.00
	7.5	7.59 ± 0.54	7.11	1.20
Extraction recoveries				
Concentration added (µg/mL)		% Extraction Recovery ± SD	% RSD	
0.08		94.19 ± 8.76	9.30	
0.15		96.51 ± 7.84	8.12	
3.5		92.01 ± 9.02	9.80	
7.5		93.93 ± 8.89	9.46	
% Stability recoveries (mean ± SD)				
Concentration added (µg/mL)	Autosampler (48 h)	Bench-top (24 h)	Long-term (2 weeks)	Freeze-thaw (3 cycles)
0.08	98.31 ± 8.52	96.95 ± 9.04	103.21 ± 5.42	99.18 ± 8.32
0.15	101.02 ± 7.43	98.72 ± 6.03	97.64 ± 9.51	98.13 ± 8.43
3.5	99.43 ± 8.03	99.31 ± 9.43	98.39 ± 8.05	100.92 ± 7.94
7.5	96.53 ± 6.05	100.93 ± 5.65	99.53 ± 6.99	98.53 ± 9.91

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383 *3.4 Physical properties of the formulated gels and evaluation of their ocular kinetics*

384 *3.4.1 Gelation temperature and viscosity of the formulated in-situ gels*

385 Factors such as gelation temperature and viscosity, particularly at different conditions, are
386 some of the most important aspects of studying thermosensitive gel preparations. Hence, we
387 assessed these properties and compared all four formulations to see the influence of Pluronic F127
388 and F88 in affecting the physical characteristics of the gels. Since the eye temperature ranges from
389 33.5 to 35.5 [28], our goal is to formulate a thermosensitive metronidazole gel that forms a gel
390 around these points.

391 In the results showing the gelation temperature (**Figure 5.IA**), it was found that all
392 preparations formed gel at different temperatures ($p < 0.05$). Formulations A and B formed gels
393 above body temperature while formulation C showed gelation at around 34.87 ± 3.12 °C.
394 Formulation D, which contains Pluronic F127 alone (20%), formed gels even lower at
395 approximately 23.64 ± 2.19 °C. The data obtained in this experiment indicated that Pluronic F88
396 as a combination of the gelling agent is required to obtain a suitable gelation temperature for eye
397 applications. This finding is also in line with the previous report stating that a combination of
398 longer hydrophobic chain poloxamers such as Pluronic F127 with more hydrophilic co-polymers
399 is essential to the formation of gelling state at the desired temperature [9,29]. **The interactions of**
400 **Pluronic F127 with the other materials such as polyethylene glycol (PEG), polyvinylpyrrolidone**
401 **(PVP), polyvinyl alcohol (PVA), methylcellulose (MC), and hydroxypropyl methylcellulose**
402 **(HPMC) have also been demonstrated as an important factor in order to control the gelation**
403 **temperature of the formulated ophthalmic sol-gel preparation [30].**

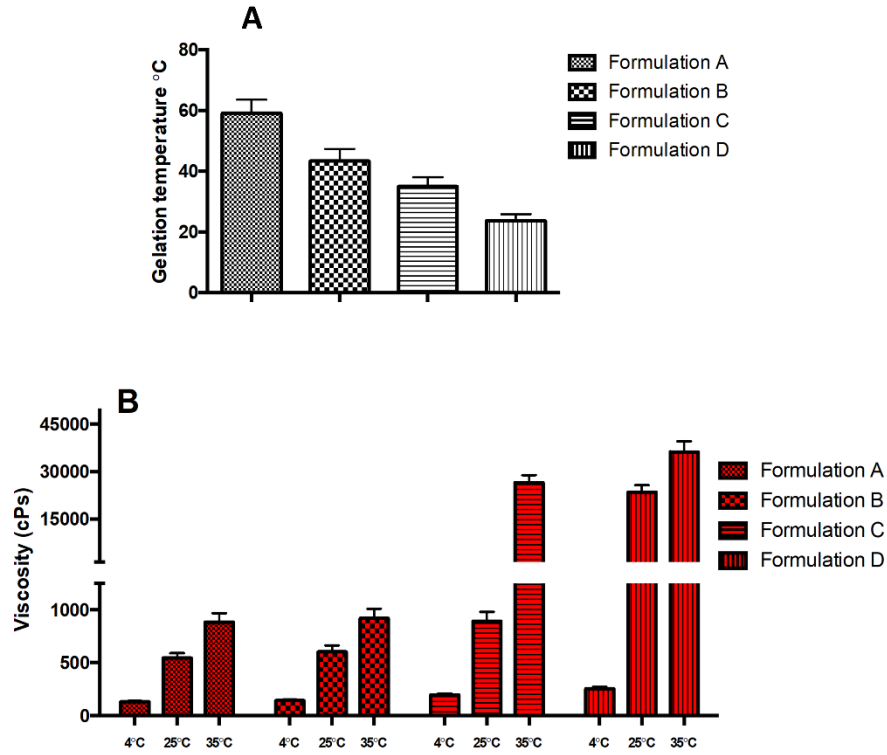
404 **In terms of viscosity,** a further investigation on the influence of Pluronic F127 and F88
405 toward **the rheology** of formulated gels also provides insight into the importance of this
406 combination on the physical properties of the gels upon application in eye or storage. As seen in
407 the **Figure 5.IB**, the viscosity of the gels increased as the temperature elevated. For instance, the
408 viscosity of formulation A and B at 4 °C was 131 ± 9.32 cPs and 143 ± 8.54 cPs, respectively.
409 When the gels are tested at room temperature, the viscosity increases, but the gelling state has not
410 been acquired. Consistent with gelation temperatures, the viscosity of Formulation C increased
411 significantly ($p < 0.05$) up to 26483 ± 2409 cPs when applied at eye temperature. In addition, this
412 formulation did not form gel upon storage at 4 and 25 °C which is considered beneficial for storage
413 conditions.

414 On the other hand, Formulation D was already in the gel form when temperature reached
415 around 25 °C, indicated by its viscosity (up to 23498 ± 2192 cPs) and even increased to around
416 36218 ± 3381 cPs at around eye temperature. No formulation was observed to form gel at 4 °C.
417 Based on these results, we agree that combination of Pluronic F127 and F88 used in formulation
418 C is the most suitable mixture of these co-polymers to obtain a thermosensitive gel for ocular
419 administration. However, we are also aware that this experiment is limited to the shorter time of
420 storage and hence a thoroughly designed stability studies should be carried out to establish effects
421 of more prolonged or even extreme storage conditions to the formulated preparations.

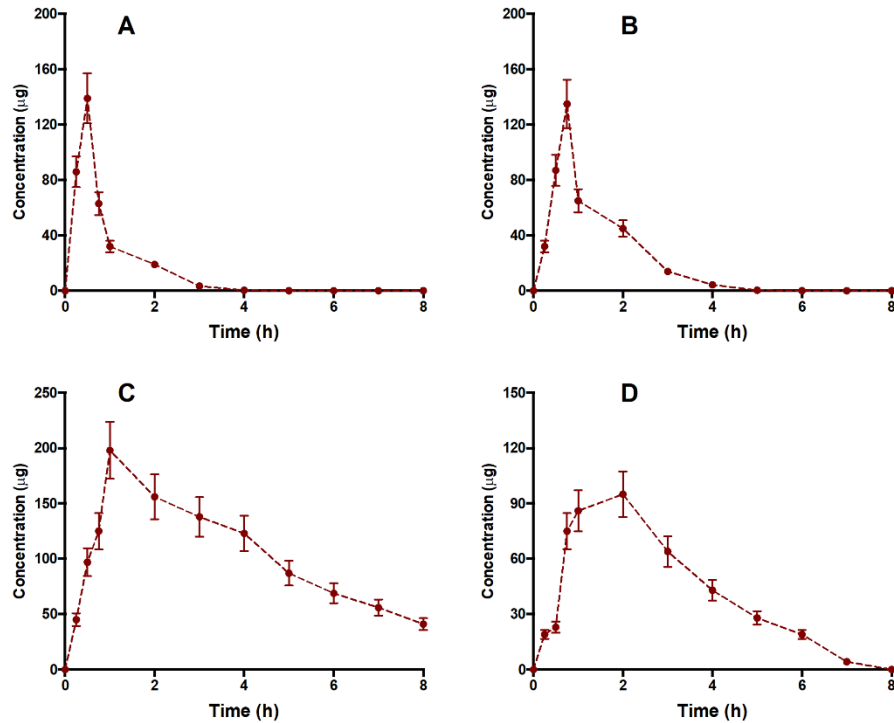
422 Pluronic F127 has longer hydrophobic poly(propylene oxide) (PPO) blocks compared to
423 its hydrophilic poly(ethylene oxide) (PEO) blocks. In contrast, Pluronic F88 has 80% PEO relative
424 to the other block chains, making this co-polymer more hydrophilic than Pluronic F127.
425 Hydrophobic PPO blocks are responsible for lowering the gelation temperature while hydrophilic
426 PEO blocks, otherwise, elevate the temperature [31,32]. A careful NMR study revealed that
427 dehydration of PPO-PEO micelles in the solution is the key for the gelation of these co-polymers
428 when applied at the specific temperature [33].

429 Although our findings mainly suggested that the use of Pluronic F127 and F88 is important
430 in the solution-to-gel formation, it is interesting to point out that other copolymers have also been
431 long utilized. For instance, in the formulation of Azithromycin thermosensitive gel, 20-22% of
432 Poloxamer 404 which contain hydrophobic PPO blocks were incorporated with 5% of Poloxamer
433 188 and 3-4% Carbopol 974P NF in order to obtain suitable gelation temperature of the ophthalmic
434 application [34]. Alkholief, M. et.al (2010) also demonstrated this effect using a similar gel base
435 in which the poloxamer and carbopol ratio was the factors that determine the slight changes in the
436 gelation temperature [35]. Another example of applicable copolymers is the use of poly-(DL-lactic
437 acid-co-glycolic acid) (PLGA)–polyethylene glycol (PEG)–PLGA as a thermosensitive gel base to
438 deliver drugs as an ophthalmic preparations [36]. All of these evidences again supported nature of
439 these polymer combinations where longer hydrophobic blocks copolymers interact with other
440 materials to obtain desired properties of the gel bases. Therefore, our study also confirmed that
441 physical characteristics such as gelation temperature and viscosity of thermosensitive in-situ gels
442 prepared using block co-polymers depend on the influence of hydrophobic and hydrophilic blocks
443 from the co-polymers.

I.



II.



444

445 **Figure 5. I.** Overall physical characteristic evaluation of thermosensitive gel preparations: (A) gelation temperature
 446 (n=3) and (B) viscosity of formulation A-D measured at 4, 25 and 35 °C (n=3); **II.** Ocular kinetic study of
 447 metronidazole thermosensitive gels showing concentration of metronidazole (µg) in corneal matrix over the measured
 448 time (hours). A-D correspond to formulation A-D which contain various types of Pluronic F127 and F88 combinations.
 449

450 3.4.2 *Ex vivo ocular kinetics evaluation of formulated metronidazole gels in corneal tissue*

451 The validated method obtained in this study was then applied in studying the ocular kinetic
452 of the formulated metronidazole gels. The kinetic profiles were obtained by evaluating the
453 concentration of metronidazole from each formulated preparation in the corneal matrix. The results
454 showing the summary of the kinetics properties of these formulations was given in **Table 2**. As
455 indicated by the data, formulation C revealed the most significant AUC value meaning the
456 metronidazole in porcine corneal availability is achieved better than the other formulations. It also
457 showed a significantly higher C_{max} ($p < 0.05$) which was reached at approximately 1 hour after
458 administration.

459 Meanwhile, this formula's half-life ($T_{1/2}$) was 2.54 ± 0.31 hours, a specific resident time of
460 metronidazole in the examined compartment. Overall, metronidazole concentrations from
461 formulation A and B were not detected at 5 hours after administration while formulation C and D
462 can extent the drug release longer (**Figure 5.II**). It is also interesting to note that formulation A
463 which contains 5% of Pluronic F127 and 15 % of Pluronic F88 reached the maximum
464 concentration of 110.81 ± 9.32 $\mu\text{g/ml}$ in approximately 30 minutes after application and the longest
465 time to reach maximum concentration was achieved by formulation D consisting of 20% of
466 Pluronic F127 and 0% Pluronic F88. The data indicate correlation between the concentration of
467 Pluronic combination (F127 and F88) and the availability of metronidazole in the cornea.
468 Increasing the concentration of Pluronic F127 in the formulation A-D seems to cause the T_{max}
469 value to be obtained at a longer time. However, there is an influence of Pluronic 127 combined
470 with F88 in enhancing the peak corneal concentration, AUC and MRT of metronidazole since the
471 half-life of formulation D which contains no Pluronic F88 cannot be solely improved by simply
472 increasing Pluronic F127 concentration. Therefore, the data presented in this study is in line with
473 our hypothesis that the combination of these two poloxamers is required in such preparations to
474 obtain better kinetic outcomes of metronidazole.

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Table 2. *Ex vivo* ocular kinetic parameters of metronidazole thermosensitive *in-situ* gels (n=3).

Parameters	Formulation A	Formulation B	Formulation C	Formulation D
C _{max} (µg)	110.81 ± 9.32	89.08 ± 8.71	171.72 ± 18.21	30.07 ± 4.31
T _{max} (h)	0.5	0.75	1	2
AUC _{0-t} (µg.h)	104.83 ± 10.21	189.59 ± 19.21	843.85 ± 90.29	37.83 ± 4.32
AUC _{0-INF} (µg.h)	104.83 ± 11.02	191.28 ± 20.12	991.36 ± 91.21	38.04 ± 3.92
T _{1/2} (h)	0.25 ± 0.02	0.78 ± 0.08	2.54 ± 0.31	0.38 ± 0.05
MRT (h)	0.69 ± 0.07	1.62 ± 0.17	4.56 ± 0.43	0.93 ± 0.12

483

484 The effect of poloxamer matrices in enhancing bioavailability of metronidazole eye
485 preparations has not been widely available, but some evidence shows that Poloxamer-based gel is
486 useful in improving ocular drug delivery of other drugs. Our previous report observed that gels
487 developed using the combination of Pluronic F127 and F68 enhance the ocular kinetic of
488 Itraconazole in an optimized thermosensitive gel preparation whether it is applied in an infected
489 or a normal eye model [9]. Pluronic F127 with other poloxamers is also known to improve the
490 availability of other incorporated drugs [37]. In terms of metronidazole delivery into eye tissue,
491 Vanderbilj [6] reported that metronidazole gel showed significant diffusion rate in human and
492 rabbit eyes compared to the eye solution. Further investigations also revealed that trans-corneal
493 diffusion of metronidazole in human and rabbit eyes is not affected by the presence of chemical
494 preservatives such as benzalkonium chloride [38]. In contributing to the previous knowledge
495 available, the experiment carried out in this study provides a new insight on the relationship
496 between poloxamer based thermosensitive gels and the kinetics of metronidazole in the eye tissue.
497 However, it is beyond our scope to evaluate the kinetic profiles of these formulations in human or
498 animal eye models even though factors such as tissue temperature and physiological conditions
499 highly influence this type of pharmaceutical preparation. Therefore, we suggested that further
500 research is carried out in addressing whether these factors are important to establish excellent
501 kinetic profiles of metronidazole in Pluronic based thermosensitive gels.

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507 **4. Conclusions**

508 The development of a validation method using this new high performance liquid
509 chromatography (HPLC-UV) method was established. The new approach developed in this study
510 in which metronidazole concentrations were measured after *ex vivo* administration in porcine
511 cornea, had high precision and accuracy, simplicity, and high sensitivity and selectivity for use in
512 therapeutic drug control research and ocular kinetics evaluation.

513 As our findings suggested, the formulation of thermosensitive gels represented in this study
514 revealed influences of PF127 and PF88 combination to produce gels with an excellent gelation
515 temperature and viscosity and their ocular kinetic properties. The method we developed here was
516 also applicable in examining the concentration of metronidazole in the formulated thermosensitive
517 in-situ gel preparations. However, further research is required to fully understand whether this
518 analysis method can also be implemented in studying the drug administration under pathological
519 conditions.

520

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523

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